



Projet Emblématique

Programme SESAME

PRAE: Platform for Research and Applications with Electrons

PRAE collaboration



*Imagerie et Modélisation
en Neurobiologie et Cancérologie*



*Institut de
Physique Nucléaire*



*Laboratoire de
l'Accélérateur Linéaire*

P. Ausset, S. Barsuk, M. Ben Abdillah, L. Berthier, P. Bertho, J. Bettane, S. Blivet, J.-S. Bousson, L. Burmistrov, F. Campos, V. Chaumat, J.-L. Coacolo, R. Delorme, N. Dosme, D. Douillet, R. Dupré, P. Duchesne, N. El Kamchi, M. El Khaldi, A. Faus-Golfe, L. Garolfi, B. Genolini, A. Gonnin, X. Grave, M. Guidal, H. Guler, P. Halin, G. Hull, M. Imre, M. Josselin, M. Juchaux, W. Kaabi, R. Kunne, M. Langlet, P. Laniece, F. Lefebvre, C. Le Galliard, E. Legay, P. Lepercq, C. Magueur, B. Mansoux, D. Marchand, A. Maroni, B. Mathon, B. Mercier, H. Monard, C. Muñoz Camacho, T. Nguyen Trung, S. Niccolai, M. Omeich, Y. Peinaud, L. Pinot, Y. Prezado, K. Pressard, V. Puill, B. Ramstein, A. Said, A. Semsoum, A. Stocchi, C. Sylvia, C. Vallerand, M.A. Verdier, O. Vitez, E. Voutier, J. van de Wiele, S. Wurth

Seminar at IHEP/UCAS, March 23, 2018

The PRAE project

- ❑ **PRAE: the multi-disciplinary site** based on the **high-performance electron beam** with the energy of **70 MeV** (intermediate PRAE version) and **140 MeV** (designed PRAE version). Infrastructure and PRAE design allows an upgrade to 300 MeV.
- ❑ **Mutually linked axes of PRAE:**
 - ❑ **Accelerator: construction of the machine to service** other axes with the beam of required performance; **accelerator R&D**
 - ❑ **Nuclear physics/nucleon structure: proton charge radius measure**
 - ❑ **Radiobiology:** new approaches in radiobiology; promising for IMRT (Intensity Modulated Radiation Therapy), radiobiology studies
 - ❑ **Instrumentation R&D: versatile instrumentation platform**
- ❑ **Re-use of the unique site of the former Linear Accelerator** and its infrastructure
- ❑ **Start of the operation** foreseen in 2020-2021.



Bruno Touschek

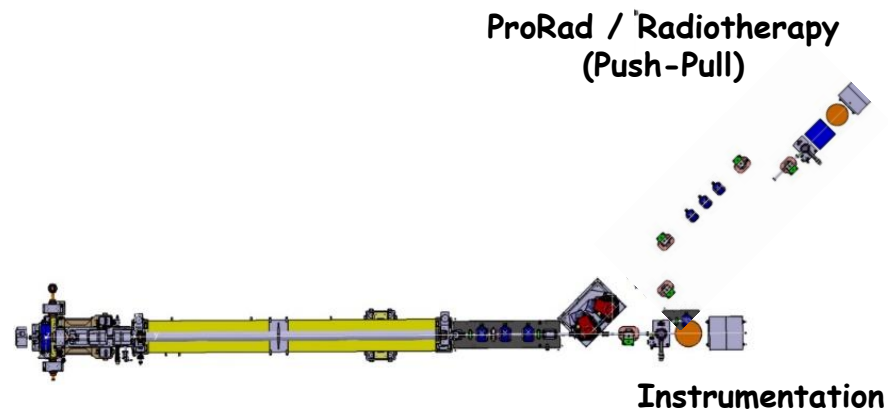
PRAE accelerator

- ❑ *Principle goal: core accelerator construction / application*
- ❑ *Other studies: R&D high-gradient RF, large intensity dynamic range BPMs, R&D on other accelerator applications*
- ❑ *Training of engineers and technical staff*

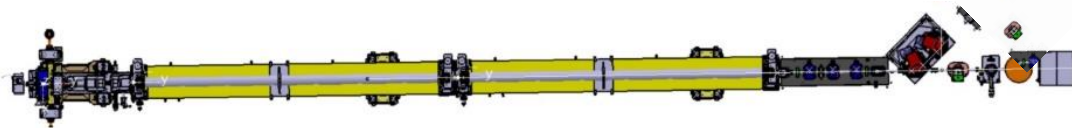
PRAE accelerator: phases of construction

Beam parameters	phase A (B)
Energy, MeV	50-70 (100-140)
Charge (variable), nC	0.00005 – 2
Normalized emittance, mm.mrad	3-10
RF frequency, GHz	3.0
Repetition rate, Hz	50
Transverse size, mm	0.5
Bunch length, ps	< 10
Energy spread, %	< 0.2
Bunches per pulse	1

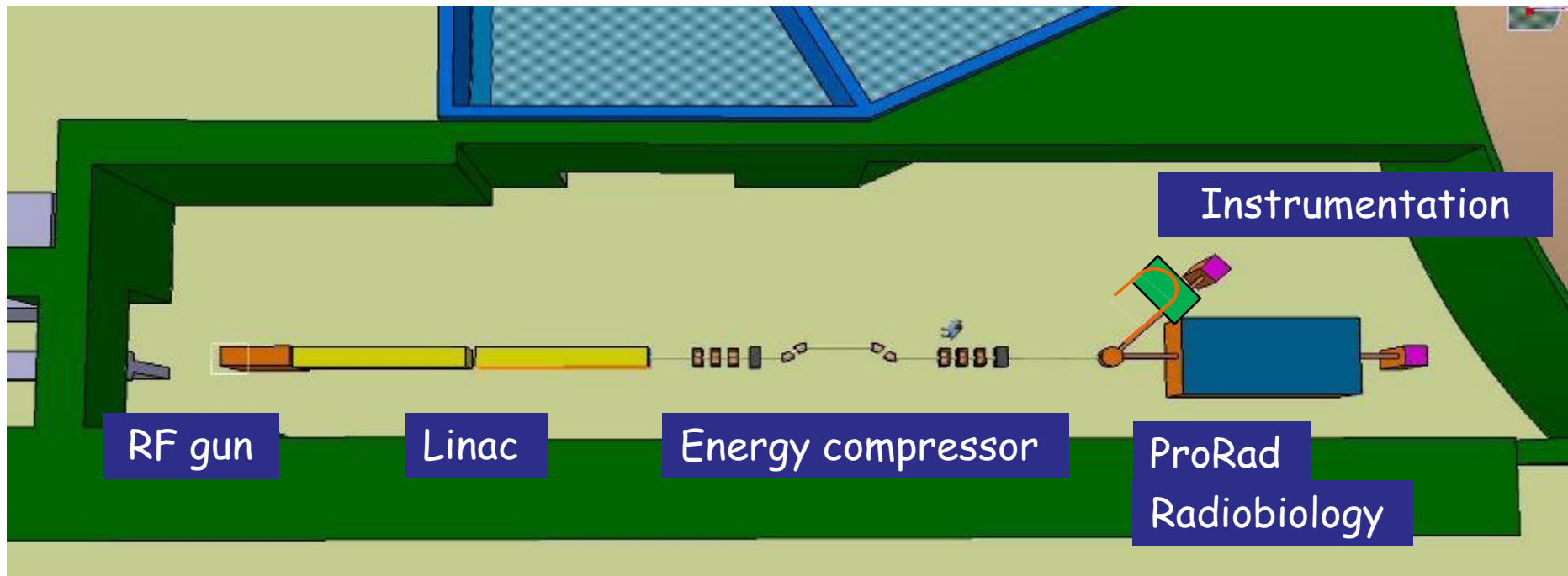
- ❑ **Phase A:** RF gun at 50 Hz; 50-70 MeV, two lines:
 - ❑ Direct for Instrumentation
 - ❑ Deviated: magnetic chicane for ProRad and radiobiology in mode "Push-Pull"



- ❑ **Phase B:**
 - ❑ Spectrometer for Instrumentation line
 - ❑ Scanning dipole
 - ❑ Complete set of channels
 - ❑ 140 MeV

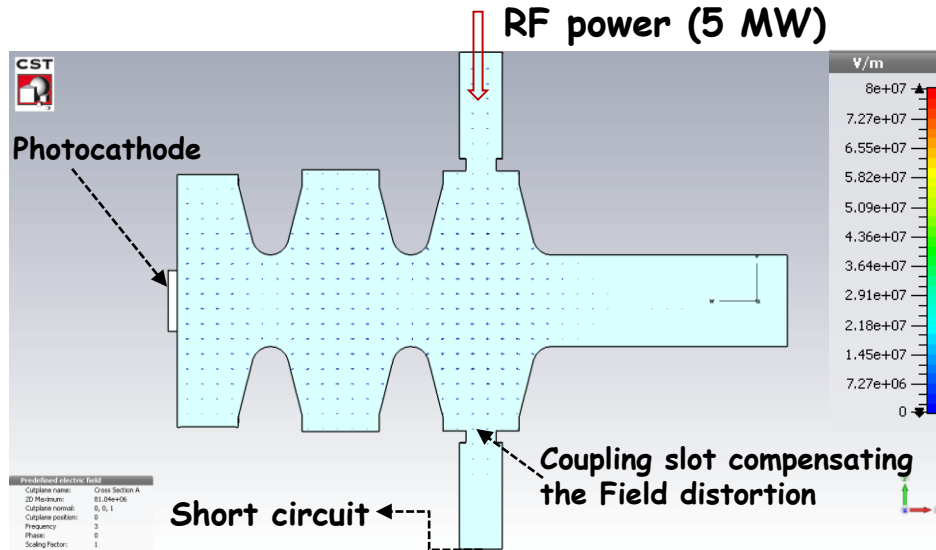


PRAE accelerator: schematic outline



LAL RF gun

Accelerating gradient ($TM_{010} - \pi$ mode):
80 MV/m at $P_{in}=5$ MW

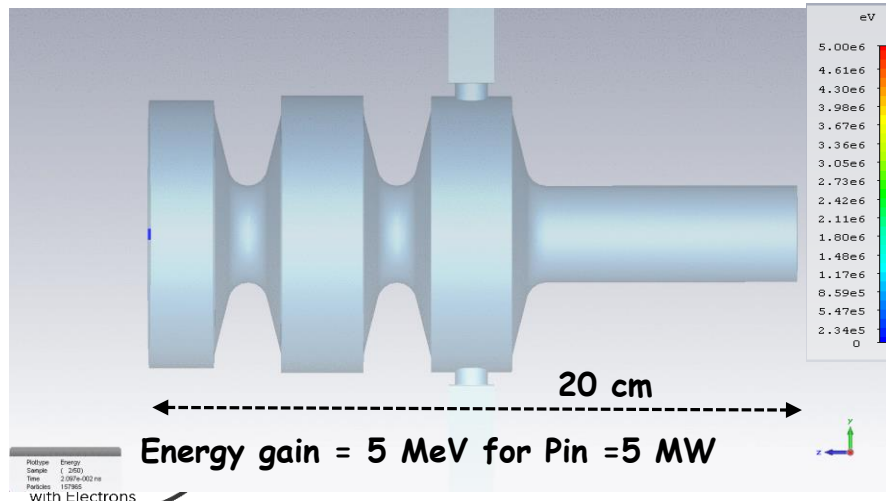


Photoinjector specification

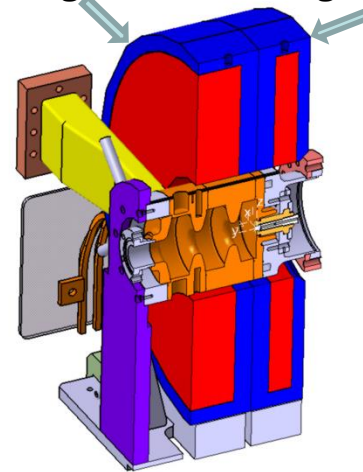
Operation frequency	2998,55 MHz (30°C, in vacuum)
Charge	1 nC
Laser wavelength, pulse energy	266 nm, 100 μ J
RF Gun Q and Rs	14400, 49 $M\Omega/m$
RF Gun accelerating gradient	80 MV/m @ 5 MW
Normalized emittance (rms)	4.4 π mm mrad
Energy spread	0.4 %
Bunch length (rms)	5 ps

2.5 cells RF gun designed and produced at LAL for ThomX

CST-Particle in cells, simulation results

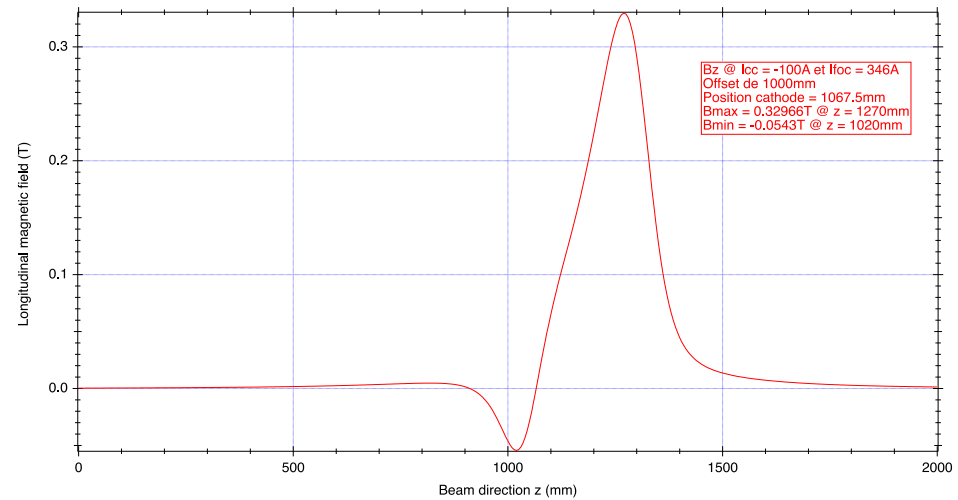
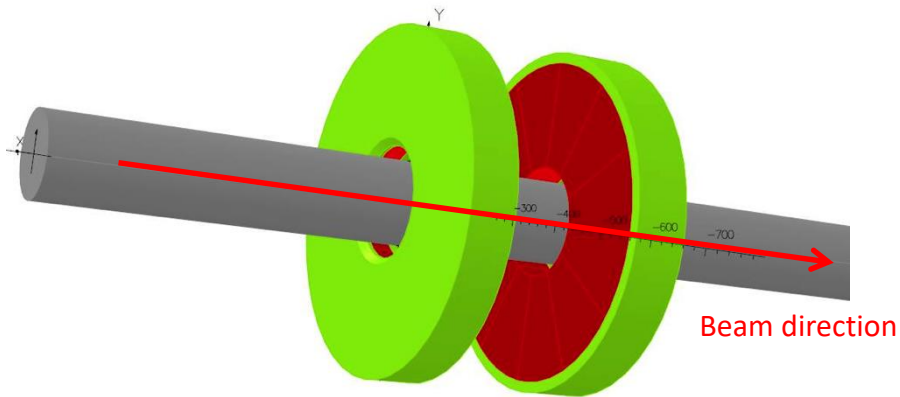


focusing coil bucking coil



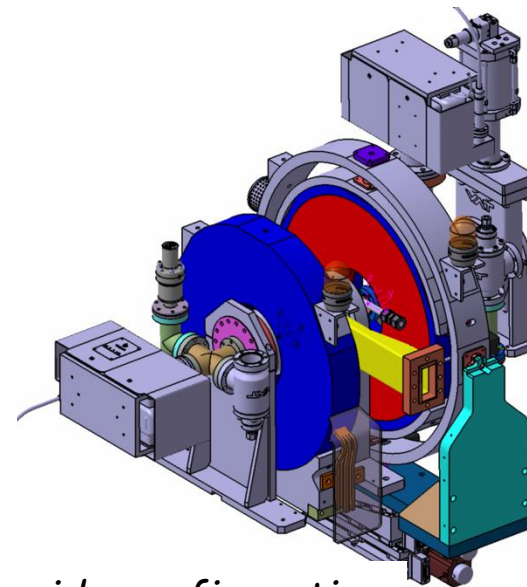
RF gun solenoids

Based on ThomX RF Gun configuration



bobine de contre champ	Pour 4 galettes de 21 spires conducteur 6x6t4 2 circuits d'eau courant de 400A			
	pression (bars)	10	15	20
	puissance (W)	12025	11518	11239
	échauffement (°C)	56.91	43.79	36.58
	débit total (l/min)	3.03	3.78	4.41

bobine de focalisation	Pour 8 galettes de 21 spires conducteur 6x6t4 4 circuits d'eau courant de 400A			
	pression (bars)	10	15	20
	puissance (W)	24051	23036	22478
	échauffement (°C)	56.91	43.79	36.58
	débit total (l/min)	6.07	7.55	8.82



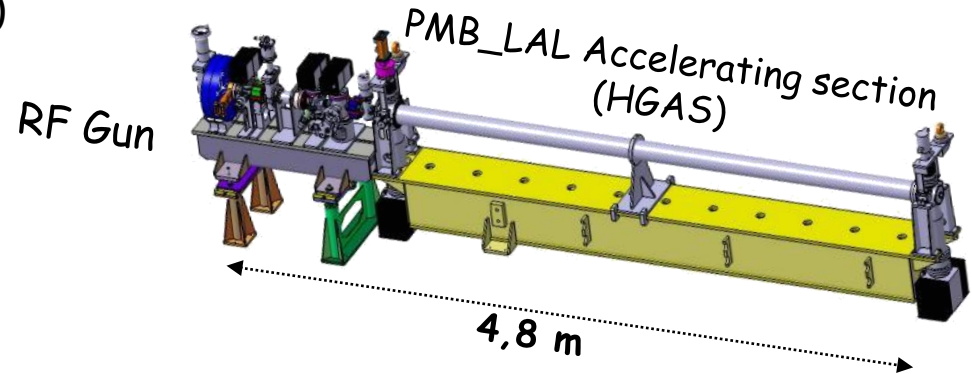
Solenoids configuration

High-gradient linac: LAL - PMB research collaboration

- High-gradient S-band compact accelerating structure development (collaboration with industry):

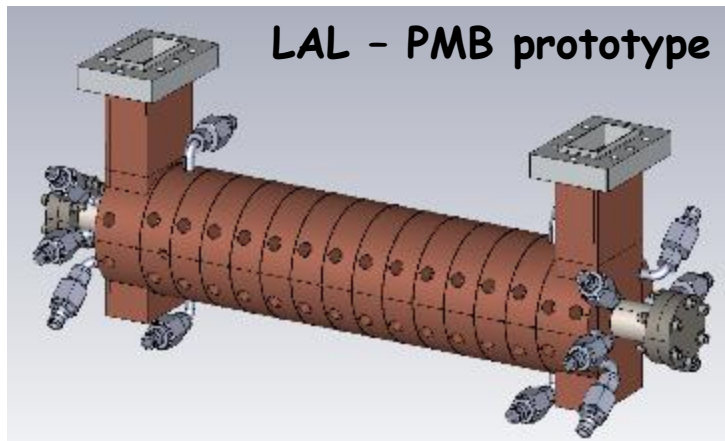
Development of high-gradient S-band TW accelerating structure (HGAS)

duration: 2014 - 2018 (4 years)



HGAS Technical specification:

Structure	Disk-loaded
Operation mode or phase advance	$2\pi/3$
Operation Frequency	2998,55 MHz (30°C, in vacuum)
Accelerator type	Quasi constant gradient, travelling wave
Accelerating Field for an input peak power of 22 MW	25 MV/m (peak value)
Energy gain for an input peak power of 22 MW	65 MeV (only HGAS)
Quality factor Q	> 14000
Number of cells	94 + 2 coupler cells
Flange to flange length	3,47 m



- ☐ RF design has been performed & main requirements accomplished
- ☐ Prototype mechanical drawings

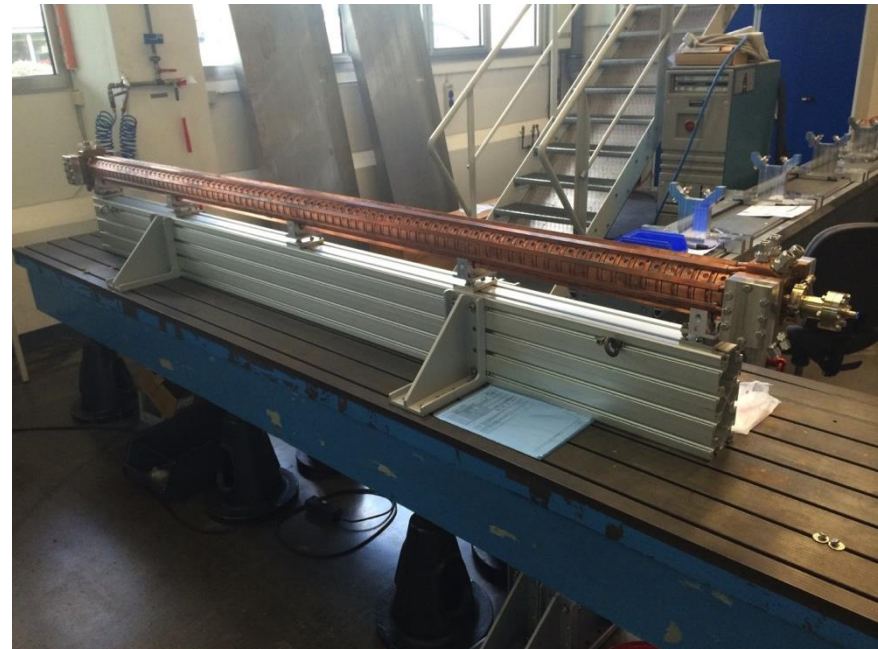
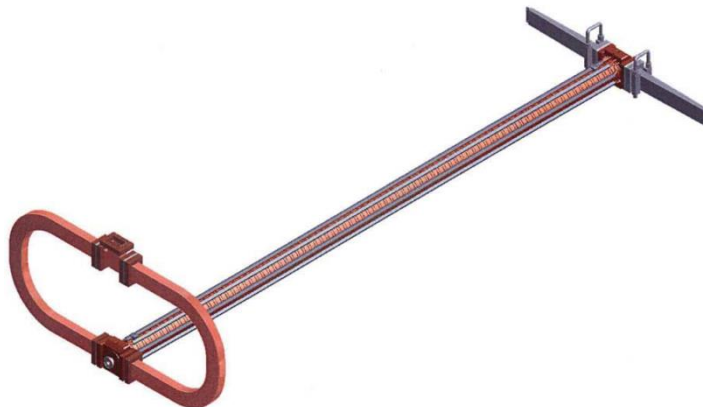
- ☐ Aluminum prototype fabrication is finished (check out & validation of all technical choices) → not validated.
- ☐ Low power tests and thermal analysis completed
- ☐ Copper prototypes will be constructed in order to validate the fabrication process
- ☐ High power tests of the Copper prototype will be done in collaboration with the IFIC HG-RF lab.
- ☐ Beam dynamics simulations of the accelerating section are underway using ASTRA and RFTrack (benchmarking)

TW S-Band structures from RI



Parameter	Value
Length	3.5m
Number of Couplers + Cells	1+96+1
Type	Constant gradient
Phase Advance	$2\pi/3$
Frequency	2998.55 @ 30° C
Pulse Width	3 μ s
Repetition Rate	50Hz
Max. input Power	40 MW
Max. average power	5 kW
Guaranteed unloaded energy gain	>65MeV

- ☐ SLAC-type structures
- ☐ Constant gradient
- ☐ Race track coupler for quadrupole compensation
- ☐ BIG Splitter for dipole compensation
- ☐ 2 RF loads



Modulator

- ❑ **RF powering:** Second generation SLAC modulator from S-band old 30 GeV linac being recuperated



Refurbished Modulator

□ RF powering: the klystron characteristics



Klystron Specifications:

Frequency Functioning mode : Pulsed
Repetition Rate : 50 Hz
Beam Pulse Width (mid-height) : $\geq 6,5 \mu\text{S}$
RF Pulse Width (flat top) : $\geq 4,5 \mu\text{S}$
Peak RF output power: $\geq 45 \text{ MW}$
Average RF output power : $\geq 10 \text{ kW}$
Nominal beam voltage : 305 kV
Nominal beam current : 340 A
Micro-perveance : 2
Efficiency (@ saturated RF output power) : $\geq 43\%$
Gain (@ saturated RF output power) : ≥ 47
Bandwidth -1dB (@ saturated RF output power): $\geq 8 \text{ MHz}$
RF input power : $\leq 500 \text{ W}$
Nominal load VSWR : $\leq 1.1:1$
Sustainable load VSWR : $\geq 1.35:1$

Focusing Electromagnet:

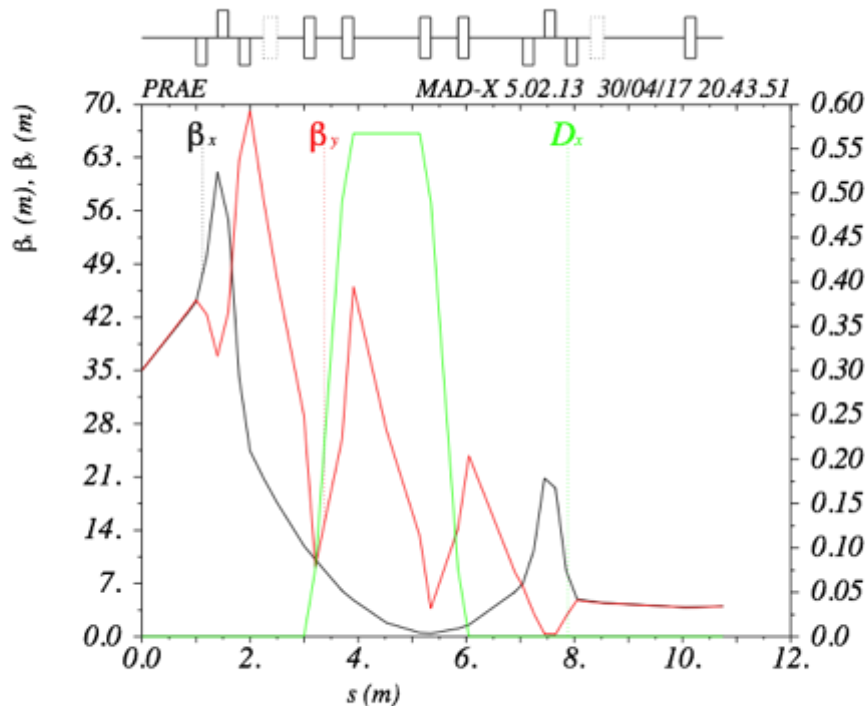
Coils : high impedance

Connections:

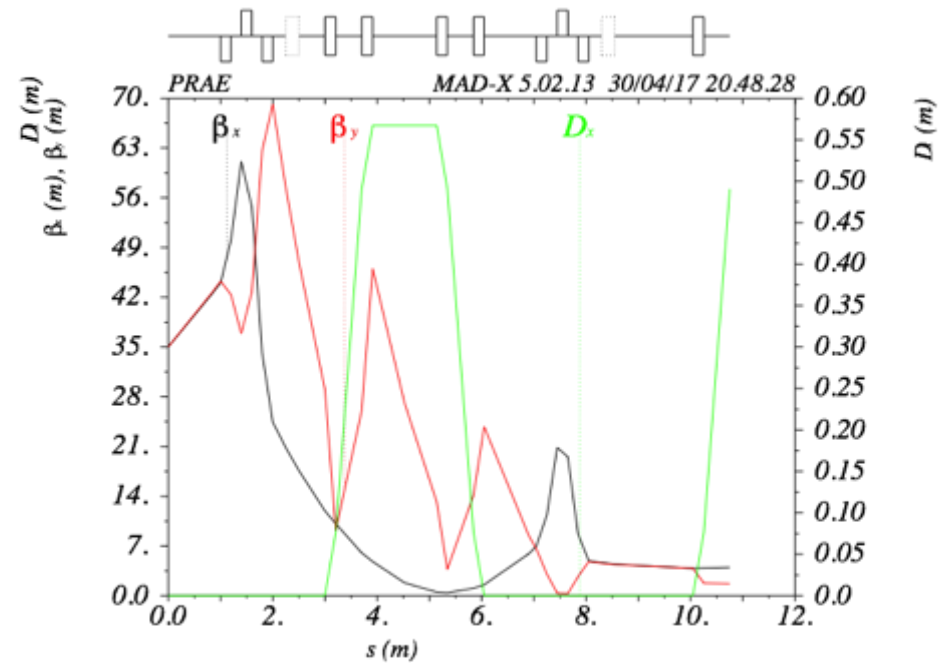
RF Input : Type N
RF Output : WR284 with crush-seal vacuum flange LIL type (use of SF6 acceptable with pressurization between 2,4 bar and 3,1 bar)

Tank oil with functionalities adapted to SLAC modulator

- Two triplets, flexible final conditions, with Energy compression System (ECS) in the direct line and a dedicated Beam Energy Measurement in the deviated line.

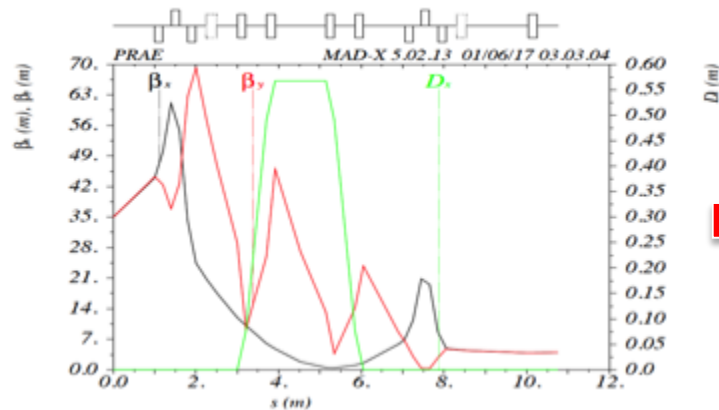


Direct line:
ProRad and Radiobiology



Deviated line:
Instrumentation

ECS dipoles (150 MeV)



Main parameters of the yoke @ 150 MeV

Gap (mm)	40
Center magnetic field (T)	1,0643
Curvature radius (°)	45
Pole width (mm)	120
Pole height (mm)	90
Yoke length (mm)	347
Yoke thickness (mm)	350
Chamfer entrance/exit (mm)	10*10

Main parameters of the coil @ 150 MeV

Ampere-turns	18000
Number of double pancakes vertical	6
Number of double pancakes horizontal	10
Number of turns	60
Current (A)	300
Conductor size (mm)	7*7
Cooling diameter conductor size (mm)	4
Number of circuits	4
Current density (A/mm ²)	8,28
Conductor length (m)	78,00
Résistance/magnet (ohm)	3,85E+01
Voltage drop/magnet (V)	23,08
Power/magnet (kW)	6,92
Number of cooling circuits	4
Water temperature rise (°C)	6
Pressure drop (bar)	7
Flow rate/magnet (l/mn)	2,24
Cooling water speed (m/s)	2,97
Reynolds number	0,03



Initial parameters :

$$\sigma_x = 6.53\text{mm} \Rightarrow \pm 8\sigma_x = 105\text{mm}$$

$$\sigma_y = 1.43\text{mm} \Rightarrow \pm 10\sigma_y = 30\text{mm}$$

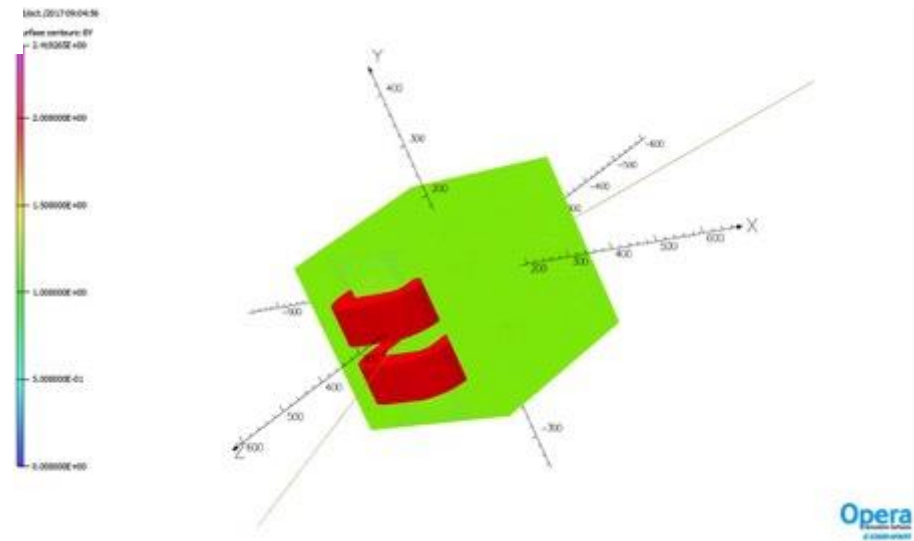
$$\text{Deviation angle} = 45^\circ$$

$$E = 150\text{MeV}$$



$$\text{GFR} = \pm 15\text{mm}$$

$$\text{Gap} = 40\text{ mm}$$



$$B1 = 1,0643\text{ T}$$

$$\text{Homogeneity} = 5.10^{-4} \text{ in the GFR}$$

$$\text{Magnetic length} = 383\text{ mm}$$

□ Pre-design is finished

Quadrupoles (150 MeV)

Initial parameters :

$R = 20\text{mm}$

$k = 28\text{m}^{-2}$

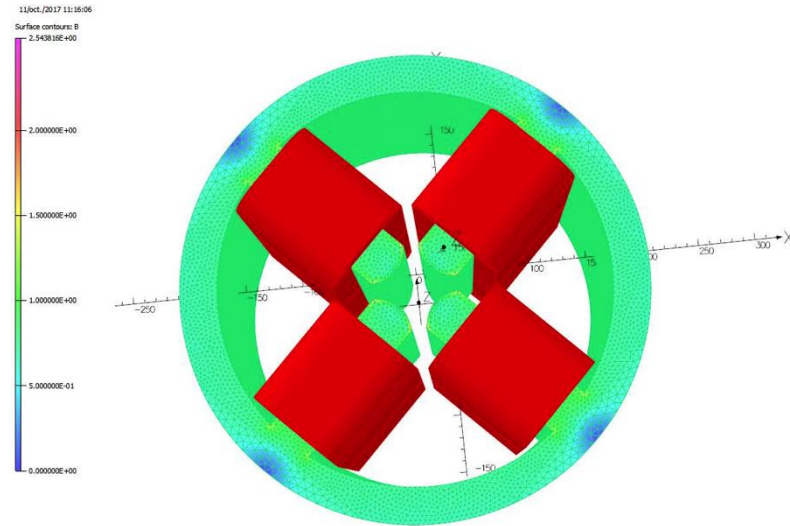
$E = 150\text{ MeV}$

Main parameters of the yoke @ 150 MeV

Gap (mm)	40
Center magnetic field gradient (T/m)	14,6059
Pole width (mm)	40
Pole height (mm)	120
Yoke length (mm)	300
Yoke thickness (mm)	190
Chamfer entrance/exit (mm)	0

Main parameters of the coil @ 150 MeV

Ampere-turns	2400
Number of double pancakes vertical	12
Number of double pancakes horizon	20
Number of turns	240
Current (A)	10
Conductor size (mm)	2*5
Current density (A/mm ²)	1,00
Conductor length (m)	194,00
Résistance/magnet (ohm)	3,26E-01
Voltage drop/magnet (V)	13,04
Power/magnet (kW)	0,13



Opera
Simulation Software
© 2008-2011

Integrated magnetic field $B_2 = -0.07063\text{ T.m}$

Magnetic gradient $G = -14.6059\text{ T/m}$

Magnetic length = 366 mm

Main harmonics :

$B_6/B_2 = -10,6$

$B_{10}/B_2 = 1,1$

$B_{14}/B_2 = 1,85$

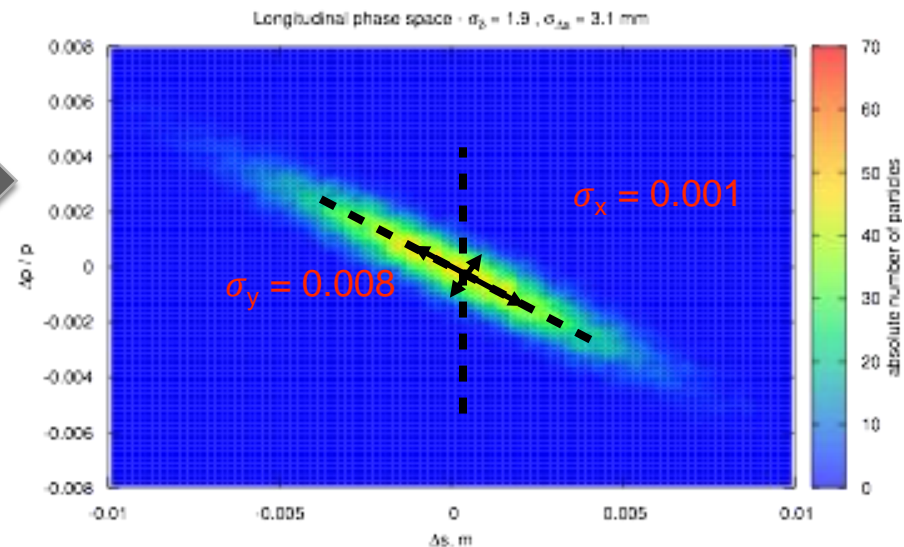
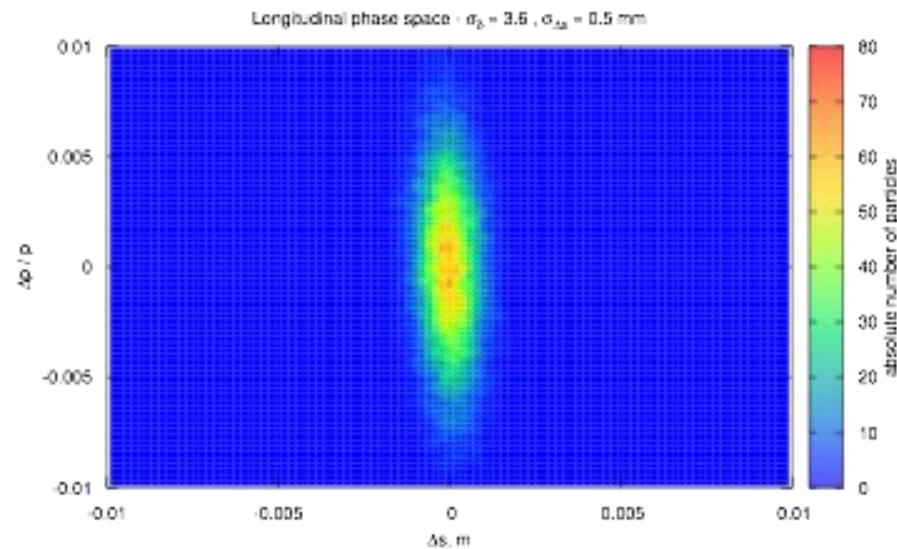
❑ Pre-design is finished. Need to optimize coils.

Initial parameters

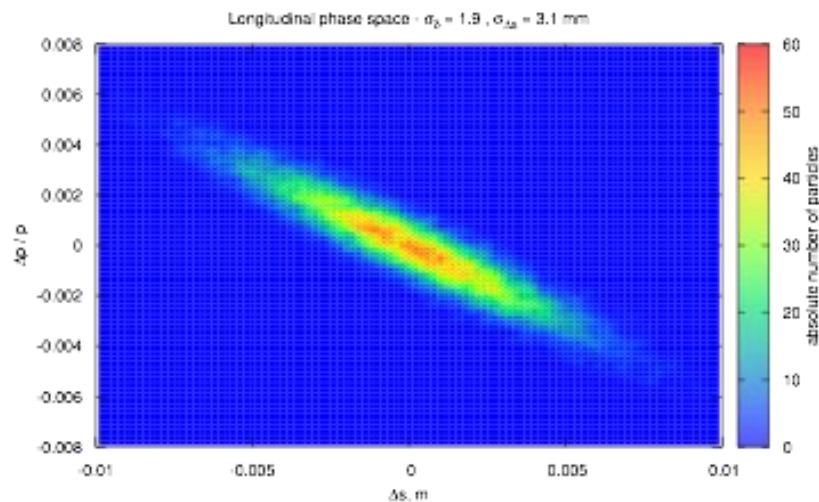
- ❑ Beam energy: 70 MeV
- ❑ Emittance: 5×10^{-8} m
- ❑ Bunch length: 3 mm
- ❑ Energy spread: 2×10^{-3}
- ❑ $\beta_{x,y} = 35$ m
- ❑ $\alpha_x = -4.24$
- ❑ $\alpha_y = -4.34$
- ❑ $D_{xy} = 0.0$

Initial distribution

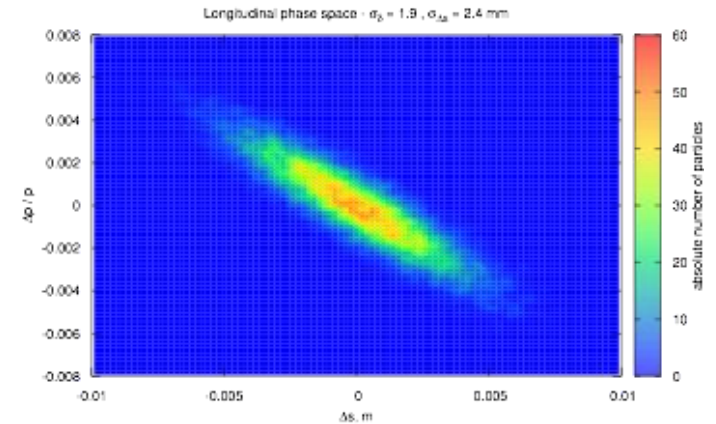
- ❑ Transverse distribution generated with 2 Gaussians, which are then rotated to simulate the energy chirp at the end of the linac, tracking with MadX-PTC in a first stage, further simulation taking into account CSR and wakefields under study.



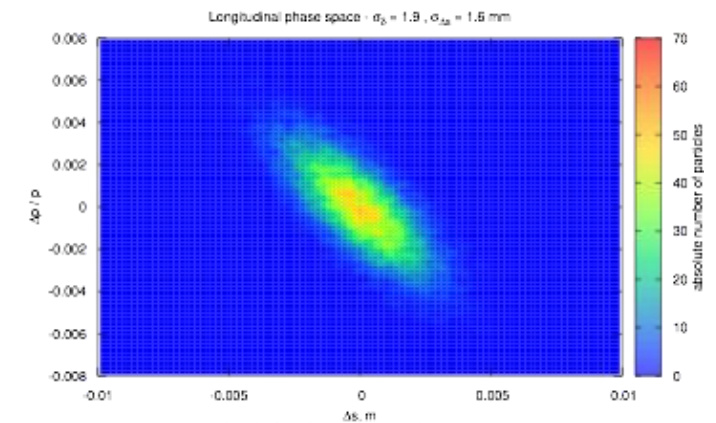
Bunch propagating through the chicane



30°

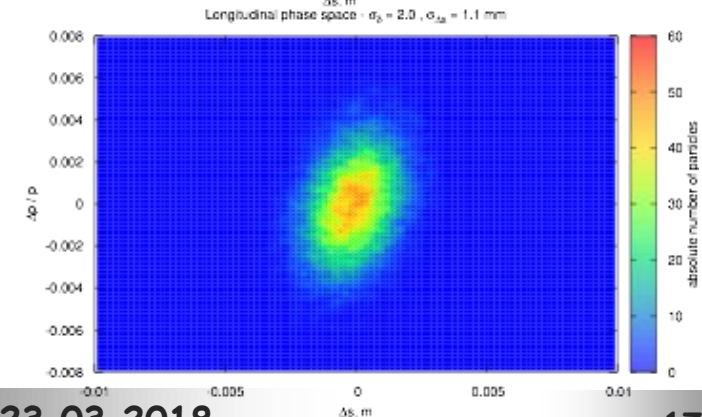


45°



Different angles 30°, 45°, 60° considered

60°

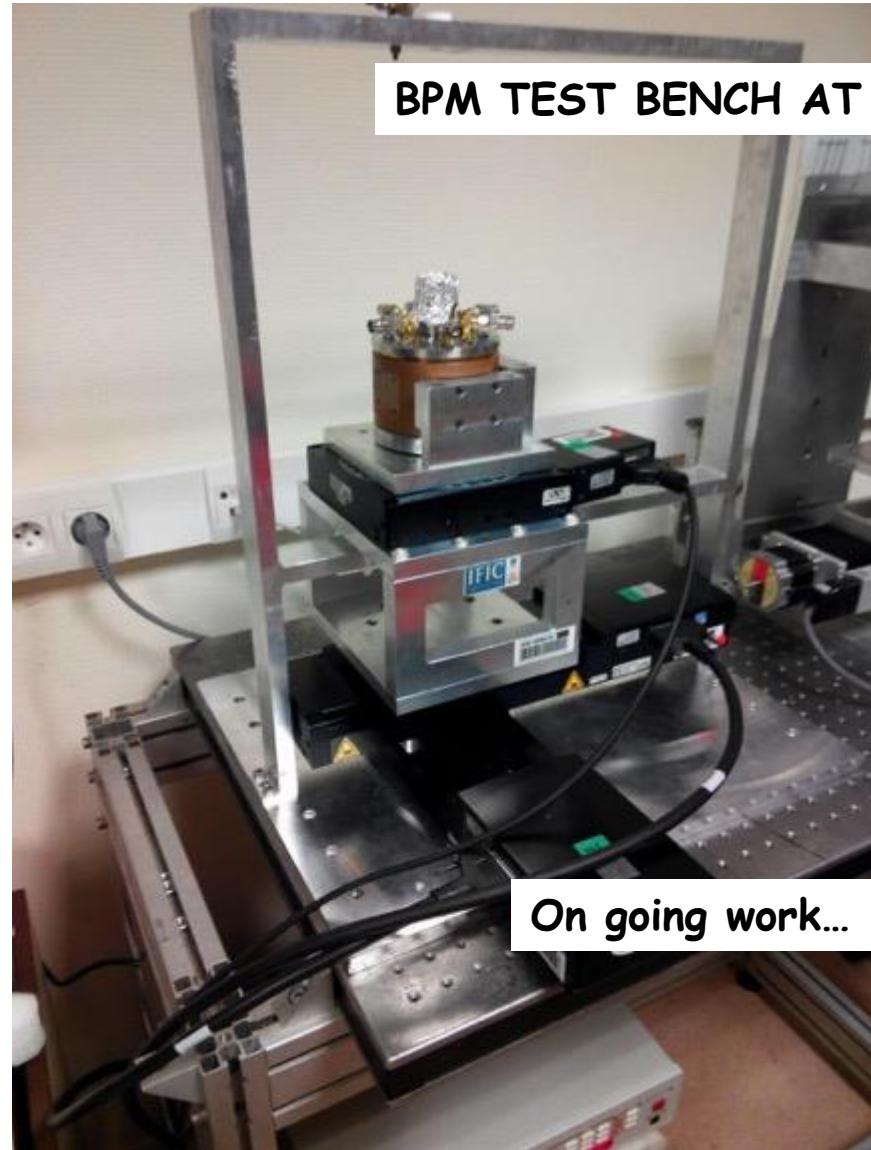
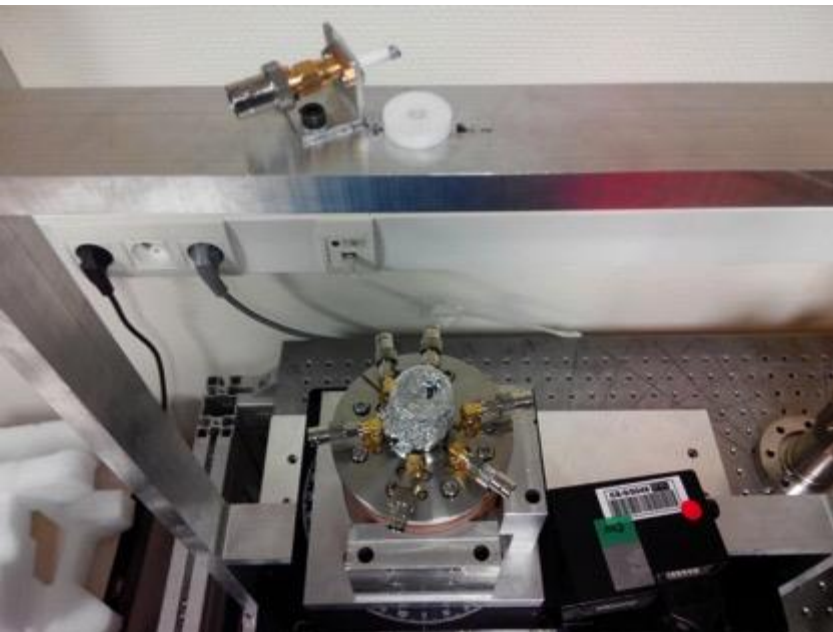


Beam diagnostics

Inductive BPMs recuperated from CTF3, tests at IPNO in collaboration with BI-CERN



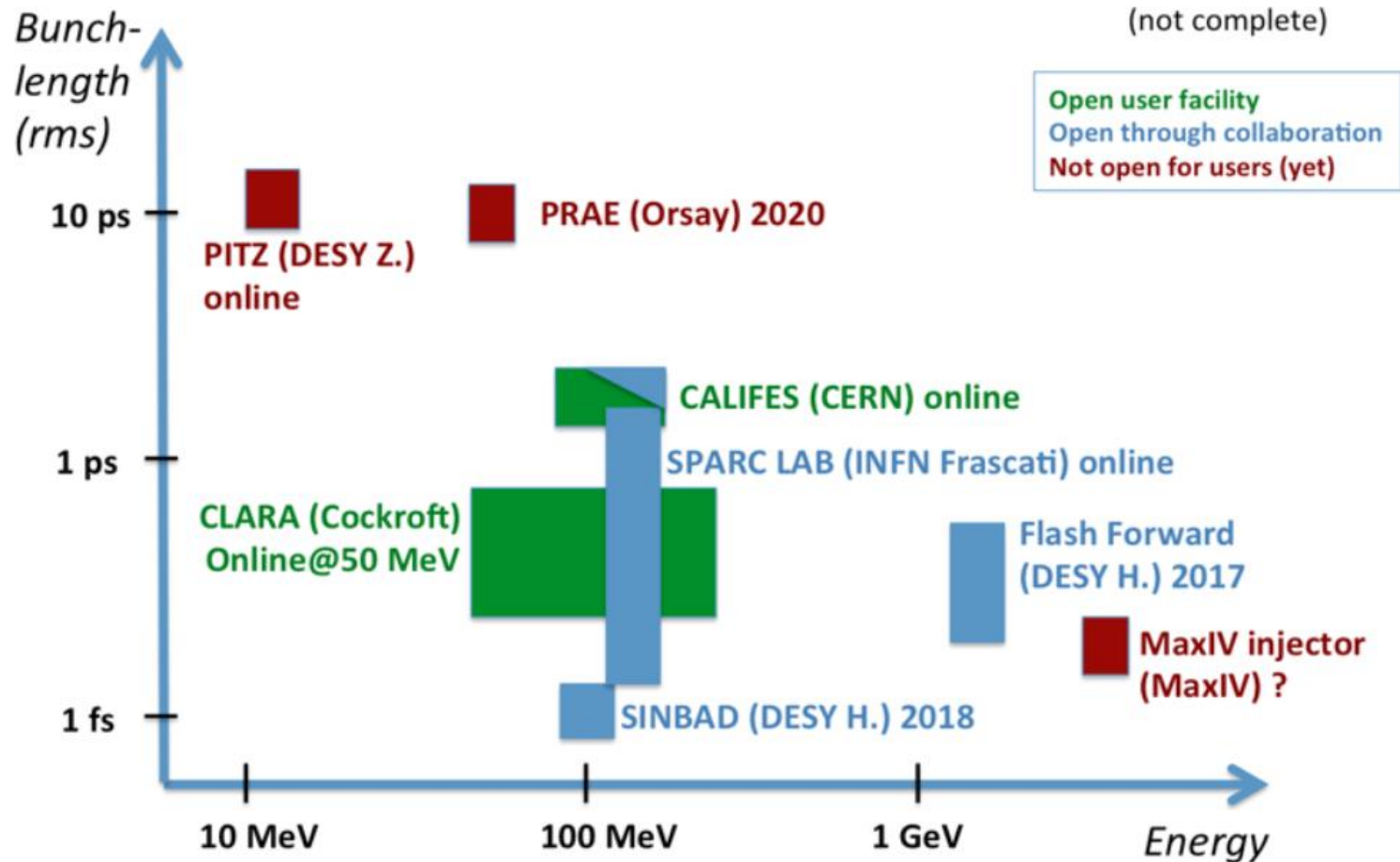
INDUCTIVE BPM



BPM TEST BENCH AT IPNO

On going work...

Present and planned European electron test beams



E. Adli - More details can be found at <https://goo.gl/sn4dqP>



Bruno Touschek

Nuclear physics / nucleon structure

- Principle experiment: *proton charge radius measurement, 30-70 MeV*



□ Determination of the proton charge radius from

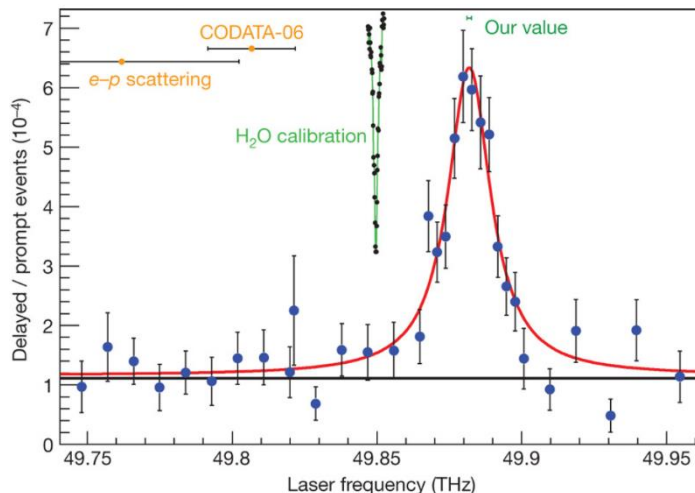
muonic hydrogen Lamb shift

significantly differs from that using

electronic hydrogen Lamb shift and electron scattering.

R. Pohl et al. Nat. 466 (2010) 213

Mesure of Lamb shift **2S- > 2P**
in muonic atom



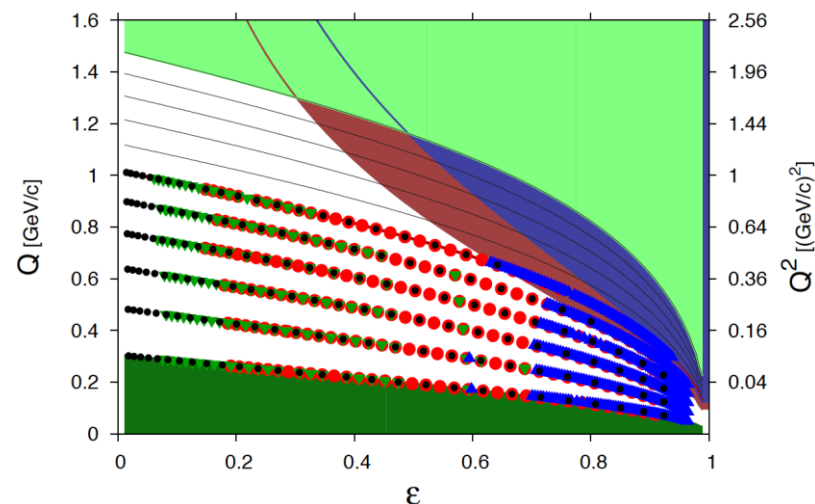
$$E_{nl} \sim -\frac{R_{\infty}}{n^2} + \delta_{l0} \frac{r_p^2}{n^3}$$

□ **Model dependence** on proton structure corrections (polarisability, 2γ) ?

□ Shift of **Rydberg** constant ?

J.C. Bernauer et al. PRL 105 (2010) 242001

Mesure of **G_E(p)** in elastic ep diffusion.



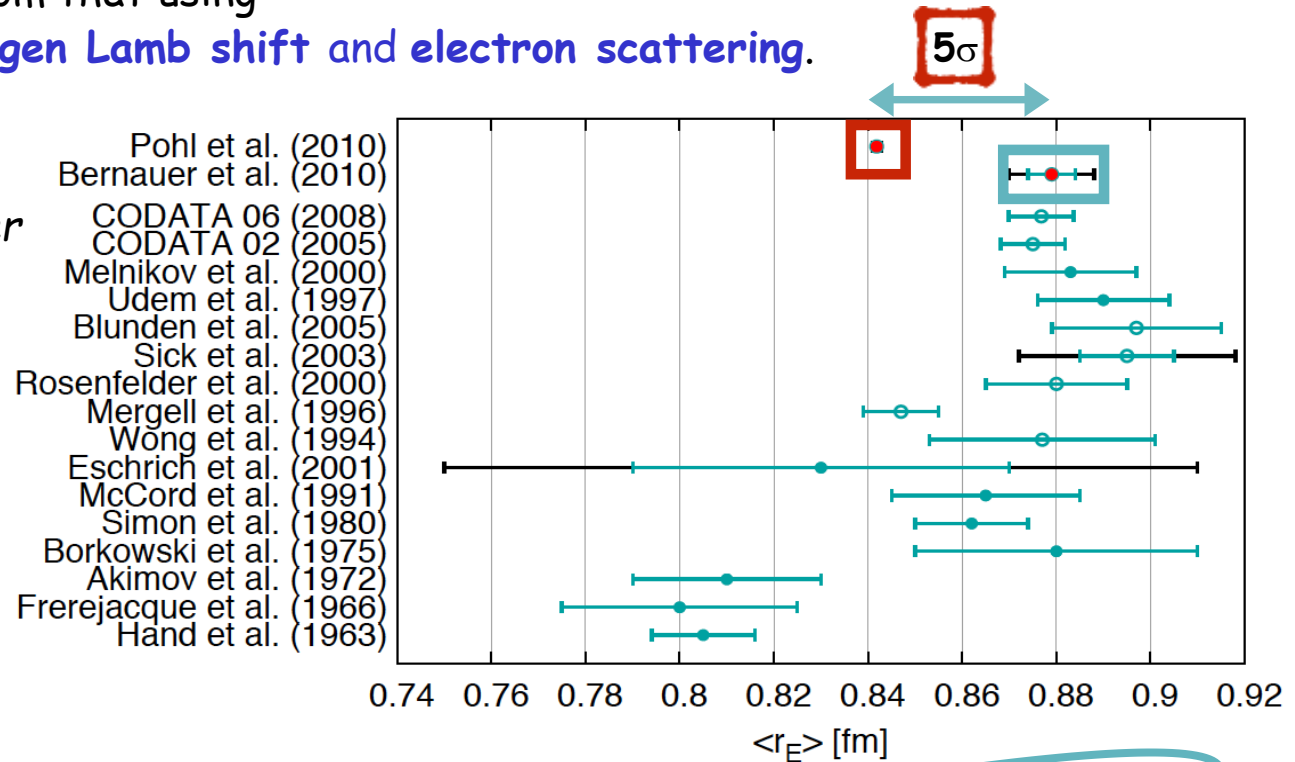
$$\langle r_p^2 \rangle = - \frac{6(\hbar c)^2}{G_E(Q^2)} \left. \frac{\partial G_E(Q^2)}{\partial Q^2} \right|_{Q^2=0}$$

□ Radiative effects and 2γ exchange ?

□ Wrong determination of r_p ?

- Determination of the proton charge radius from **muonic hydrogen Lamb shift** significantly differs from that using **electronic hydrogen Lamb shift and electron scattering**.

The **proton** looks smaller to **muons** than to **electrons**.



$$r_p = 0.84184 \pm 0.00067 \text{ fm}$$

Direct measurement
(10 times more precise)

$$r_p = \sqrt{\langle r^2 \rangle} = \sqrt{-6 \frac{\partial G_E^2(Q^2)}{\partial Q^2} \Big|_{Q^2=0}}$$

$$r_p = 0.87900 \pm 0.00800 \text{ fm}$$

Indirect measurement
(extrapolation of FF data to $Q^2=0$)

- Search for **explanations from experimental issues, theory, ...** : Underestimated uncertainties / Bad radius determination / Lepton non-universality / New force/particles / Novel hadronic physics / ...

□ Problem maybe related with

B physics anomalies: experimental results \neq SM predictions!

charged current SM tree level

$$R_{D^{(*)}} = \frac{BR(B \rightarrow D^{(*)} \tau \nu_\tau)}{BR(B \rightarrow D^{(*)} \mu \nu_\mu)} \quad 3.9\sigma$$

$$\frac{BR(B_c \rightarrow J/\Psi \tau \nu_\tau)}{BR(B_c \rightarrow J/\Psi \mu \nu_\mu)} = 0.71 \pm 0.17 \pm 0.18 \quad \begin{array}{l} 13 \text{ Sept. 2017} \\ \text{LHCb result} \\ \sim 2 \sigma \end{array}$$

FCNC - SM loop process

P_5' in $B \rightarrow K^* \mu^+ \mu^-$ (angular distribution functions) 3σ

$$R_{K^{(*)}} = \frac{\Gamma(B \rightarrow K^{(*)} \mu^+ \mu^-)}{\Gamma(B \rightarrow K^{(*)} e^+ e^-)} \quad \begin{array}{l} \text{in the dilepton invariant mass bin} \\ 1 \text{ GeV}^2 \leq q^2 \leq 6 \text{ GeV}^2 \\ \sim 4\sigma \end{array}$$

Muon anomalous magnetic moment

$$a_\mu^{\text{exp}} = 1.16592080(63) \times 10^{-3}$$

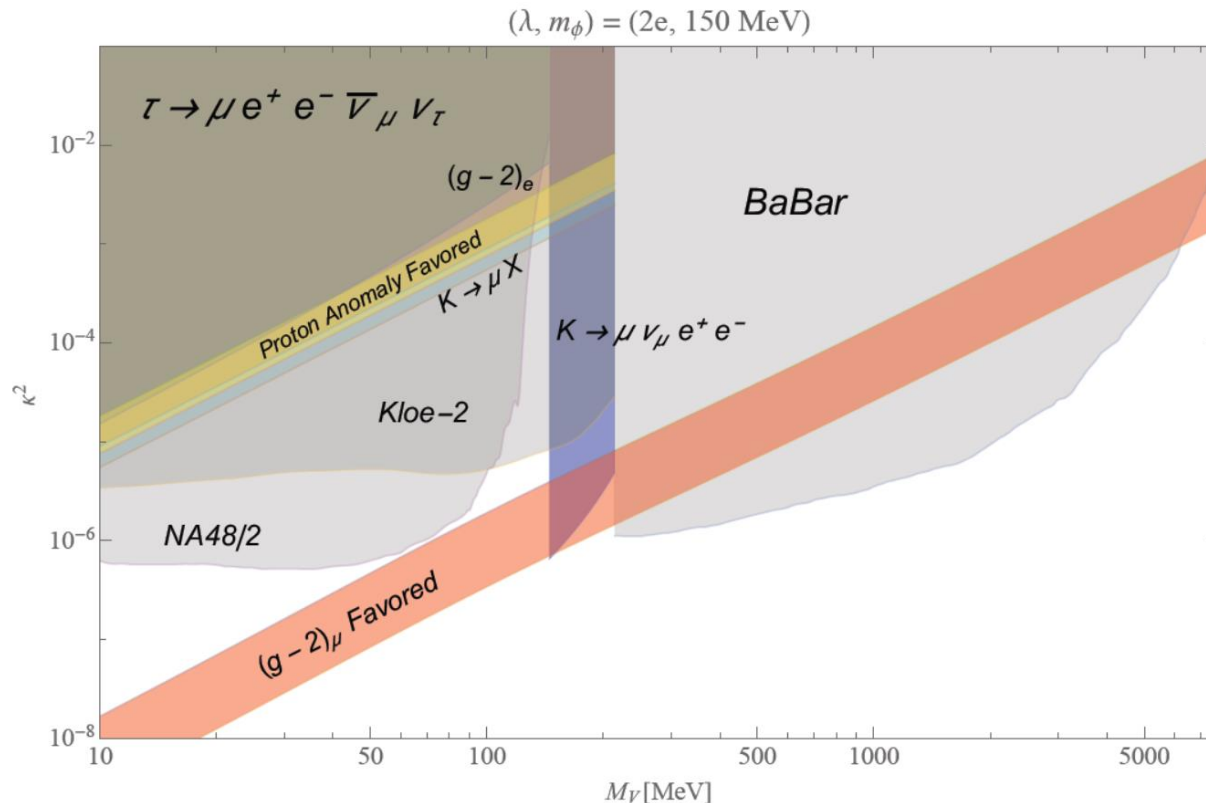
$$a_\mu^{\text{SM}} = 1.16591803(70) \times 10^{-3}$$

$$\Delta a_\mu = (2.8 \pm 0.9) \times 10^{-9} \quad \sim 3\sigma$$

S. Fajfer

Model of DM (F. C. Correia, S. Fajfer, arXiv:1609.0860, Batell et al., arXiv:1103.0721):

- V is the gauge boson, neutral under the SM gauge group and charged under $U(1)_d$
- κ is a mixing angle between dark boson and photon

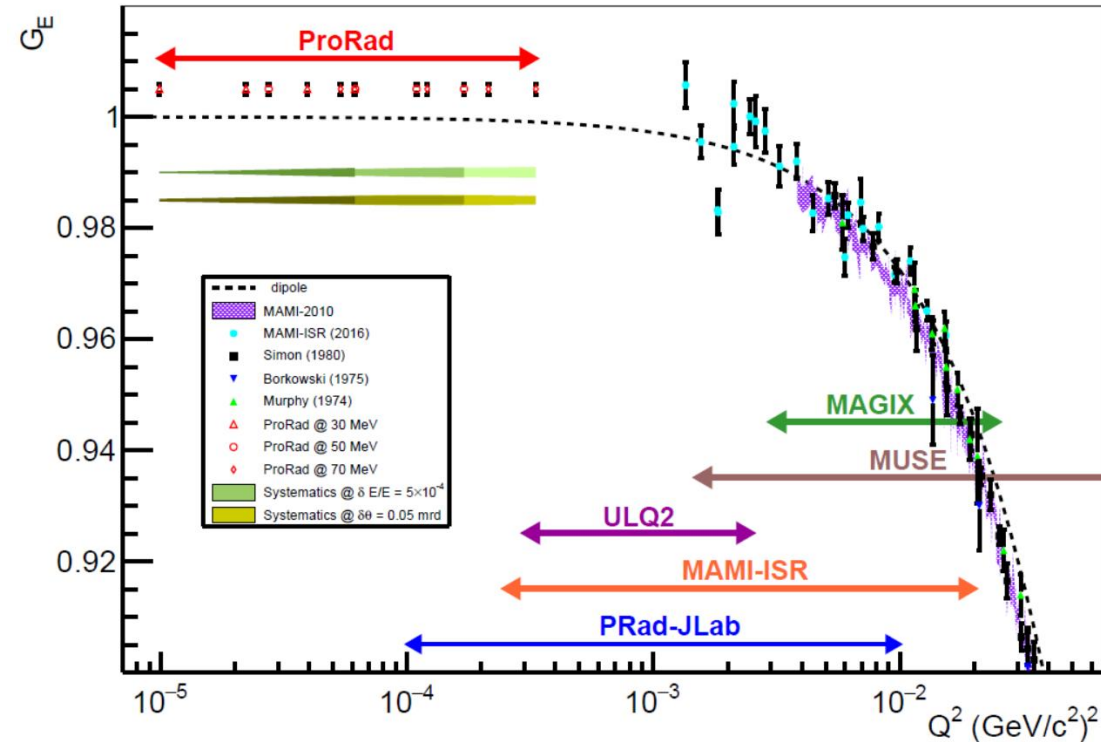


- Colour areas are excluded (for proton charge radius and $(g-2)_\mu$ yellow and red are favored)!

- ❑ The **ProRad** experiment at **PRAE** aims at accurate measurements ($\leq 1\%$) of the electric form factor of the proton $G_E(Q^2)$ at **very low** four-momentum transfer Q^2 .

$$\frac{d^2\sigma}{d\Omega} \equiv \frac{d^2\sigma}{d\Omega} \Big|_{\text{Mott}} G_E(Q^2) \longrightarrow r_p^2 = - \frac{6\hbar^2}{G_E(0)} \frac{\partial G_E(Q^2)}{\partial Q^2} \Big|_{Q^2=0}$$

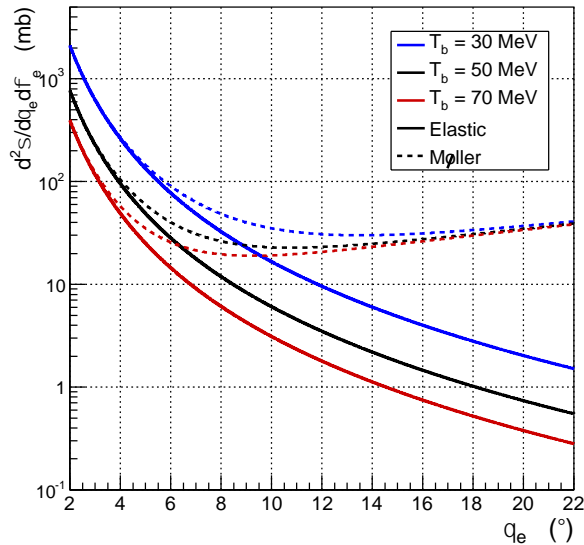
A linear region in the FF: extrapolation with no dependence on non-linearities



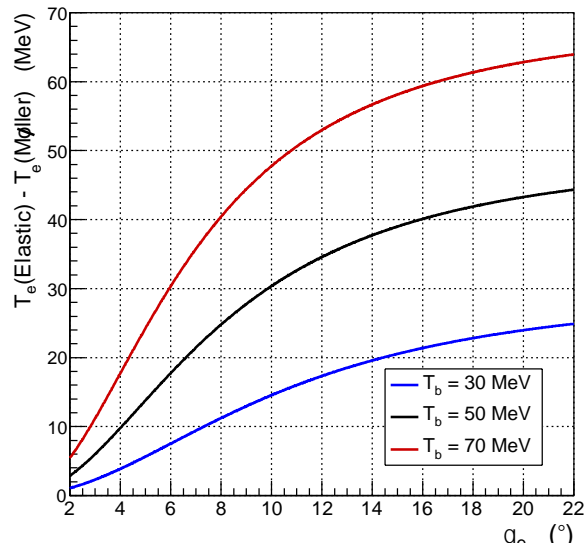
- ❑ Measurements in the **unexplored** Q^2 -range $1.5 \times 10^{-5} - 3 \times 10^{-4} \text{ (GeV/c}^2\text{)}^2$ will **constrain** the Q^2 -dependence of G_E and the **extrapolation to zero** important for the determination of the **proton charge radius**.

- ❑ Any deviation from 1 would indicate **genuine novel effects**.

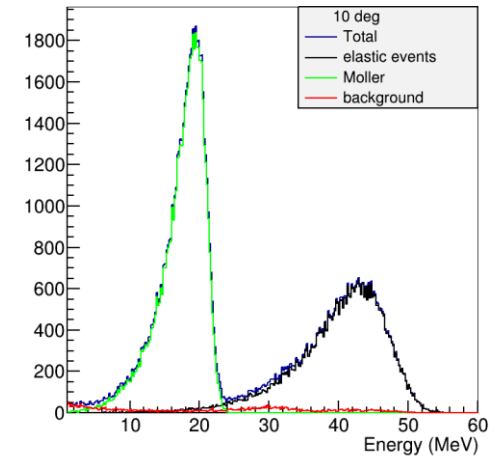
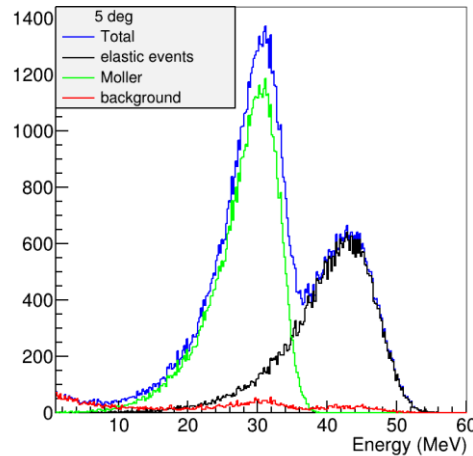
Differential Cross section



Energy Separation



- Measurements of the **ep elastic** scattering between **5°** and **15°** (5 angle points) at 3 different beam energies, and in **absence** of any **magnetic field** (and tracking system ?).
- The **energy deposit spectra** in calorimeter allow separation between **elastic** and **Møller** electrons



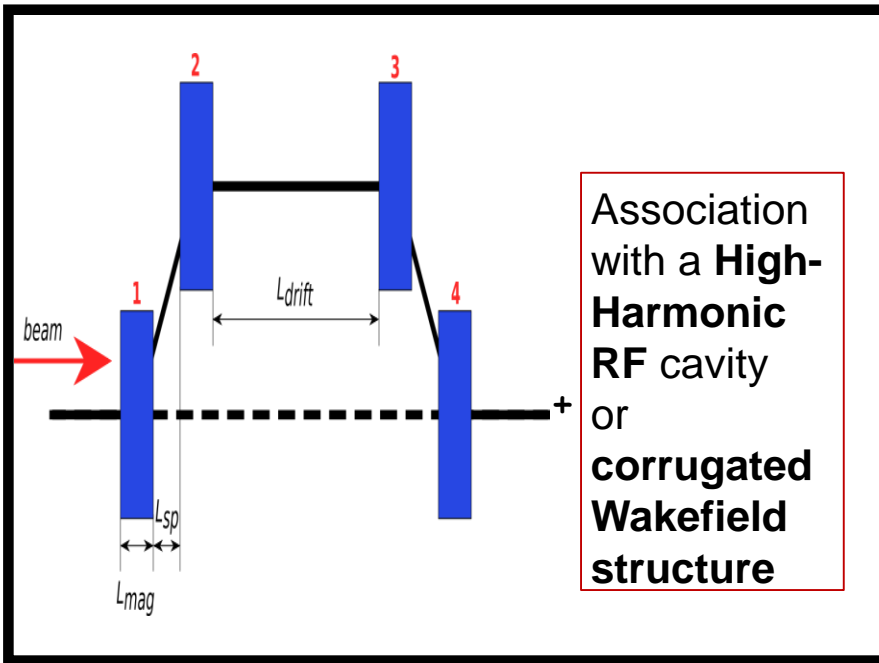
- Absolute **normalization** from **simultaneous** measurement of **ep elastic** and **ee Møller** within the **same detector** using scattered electron kinematic separation.
- **Precise beam**:
 $\Delta E/E = 10^{-3}$, $\sigma_{x,y} < 0.5$ mm, $\Delta\theta < 1$ mrad

ProRad experiment requirements

- ❑ High precision beam: **Reduced energy dispersion** $\delta P/P = 5 \times 10^{-4}$
- ❑ Precise knowledge of the beam energy $\delta E/E = 3 \times 10^{-4}$
- ❑ A stable target
- ❑ Optimized measurement of the scattered electron energy and position

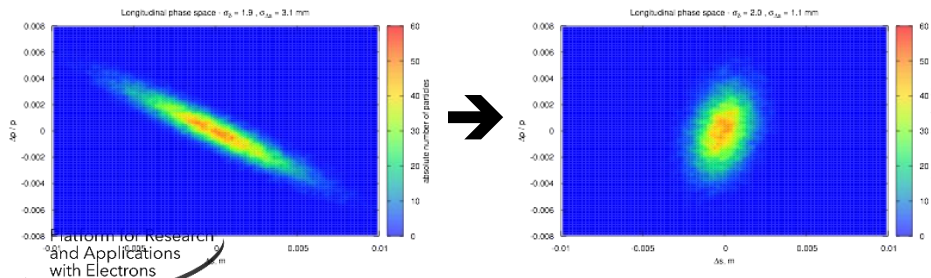
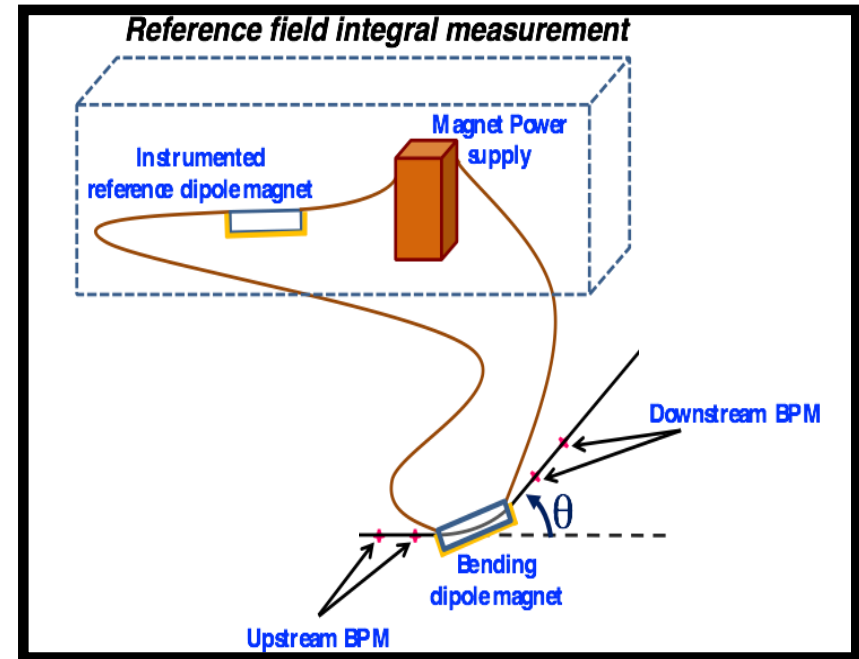
$$E = \frac{c}{\theta} \int B dl = \frac{c}{\theta} I_B$$

Energy compression



+

Beam energy measurement



$$\frac{\delta I_B}{I_B} = \frac{\delta \theta}{\theta} = 2 \times 10^{-4}$$

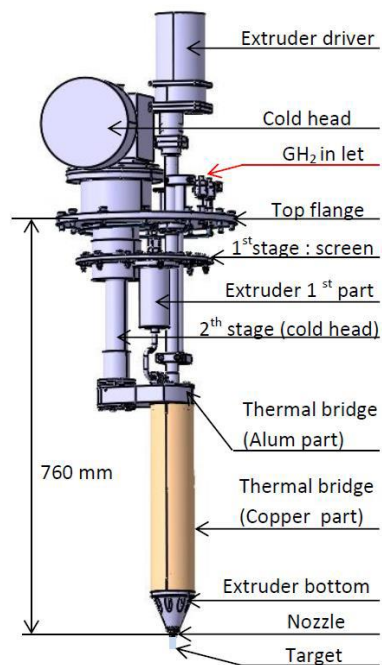
Hydrogen target

- ❑ Selection of reliable target of acceptable cost: **CHyMENE** film (CEA Saclay), **solid wire** from techniques of droplet beam (Frankfurt am Main University), ...

J.-M. Gheller et al. AIP Conf. Proc. 1573 (2014) 58

A. Gillibert et al. EPJA 49 (2013) 155

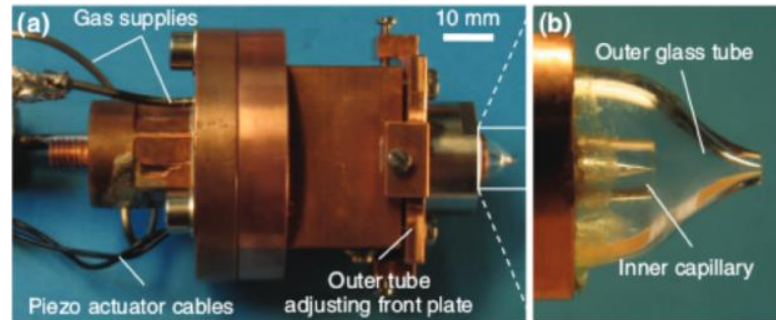
Cryogenic system in the cryostat



CHyMENE

*Bi-national ANR proposal with
Frankfurt University submitted.*

Droplet Stream



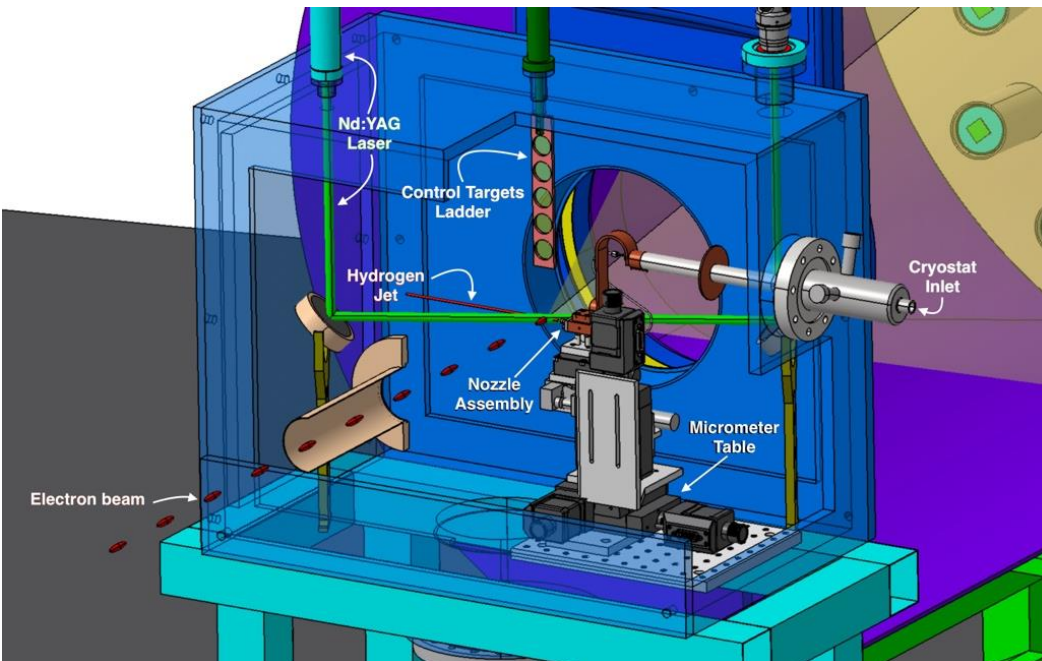
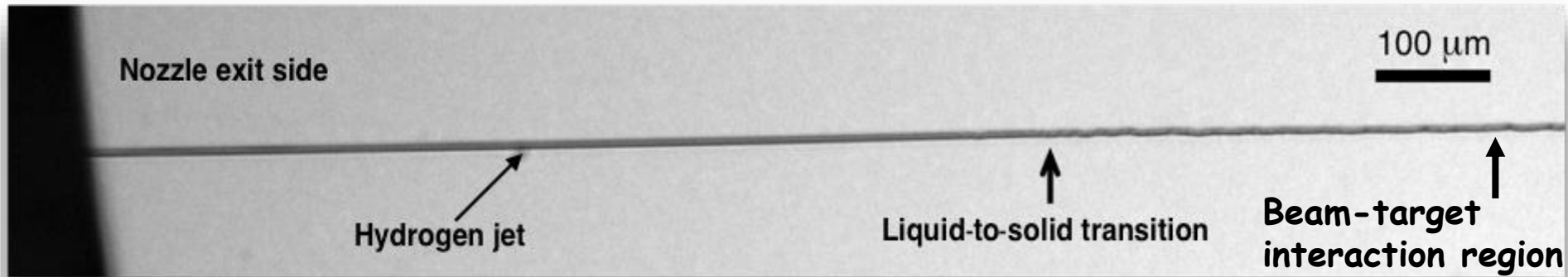
R.A. Costa Fraga et al. Rev. Sci. Inst. 83 (2012) 025102

- ❑ Hydrogen film of **50-200 μm** produced via extrusion technique.
- ❑ Adaptation needed to achieve **$\sim 20 \mu\text{m}$** .
- ❑ Complementary system based on **conventional solid targets** for beam control and check for systematics effects.

Hydrogen target

Requirements:

A very stable, windowless, and self-replenishing target of 15 μm diameter

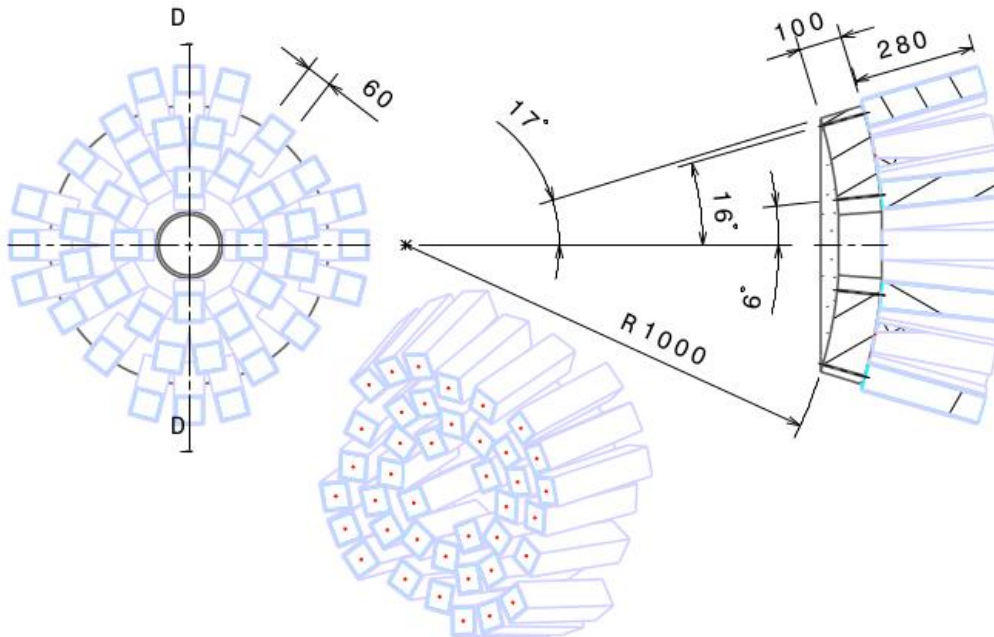


Ultra cold liquid technology
developed at Frankfurt University

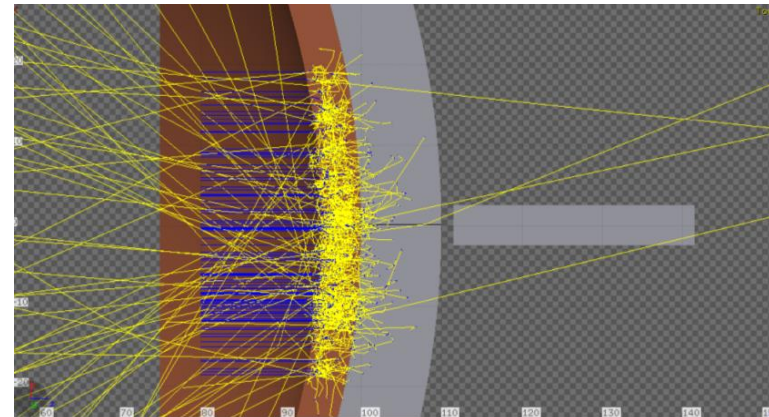
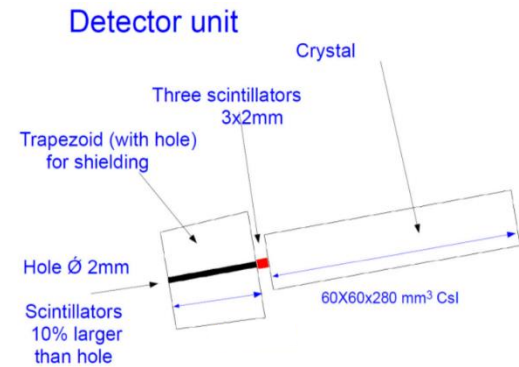


Detector

- ❑ Conceptual studies with GEANT4 and FLUKA to **optimise detector configuration for small diffusion angles**.
- ❑ BGO crystals for energy measurements and fiber tracker to measure position
- ❑ Studies of **system mechanics**.



Cristaux de 6 cm + 5 mm de boitage
Inclinaison angulaire = 6° - 8.5° - 11° - 13.5° - 16°





Bruno Touschek

Radiobiology

- ❑ *Principal goal : explore new original approaches in radiotherapy*
- ❑ *Other studies : promising for IMRT, radiobiology studies*

New approaches in radiotherapy

- ❑ Radiotherapy (RT) is one of the most frequently used methods for **cancer** treatment
- ❑ Treatment of some **radio resistant tumors**, **pediatric cancers** and tumors close to a delicate structure (i.e. spinal cord) is currently **limited**
- ❑ The main challenge is to find **novel** approaches to increase normal tissue resistance
- ❑ Standard RT restricted to the few temporal and spatial schemes, dose rates, broad field sizes: mainly photons, 2 Gy/session, 1 session/day, 5 days/week, dose rates ~ 2 Gy/min, field sizes $> \text{cm}^2$, homogeneous dose distributions

Possible strategy to spare normal tissue: VHEE

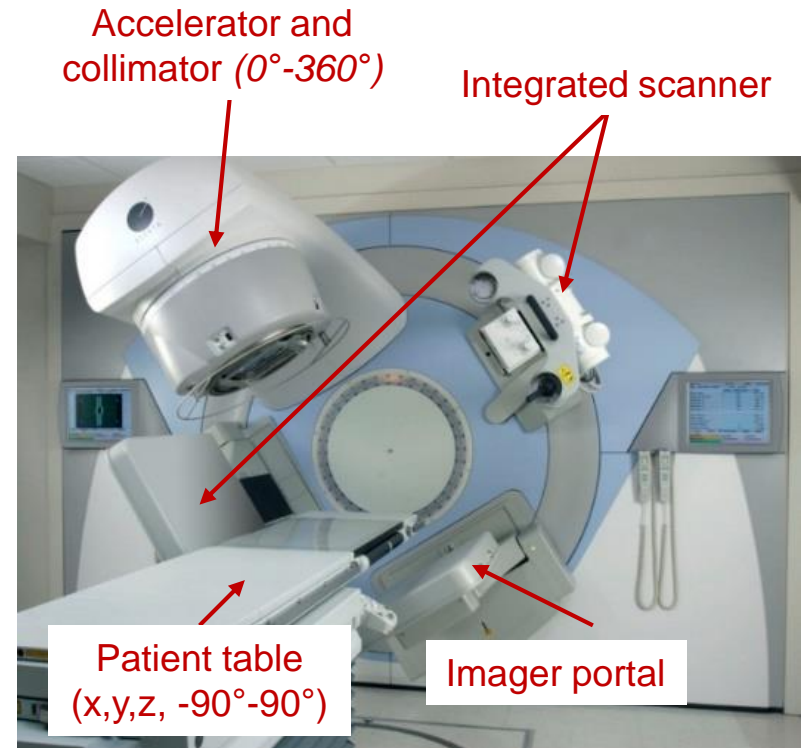
- ❑ Different particle types: very high energy electrons (VHEE)
 - ❑ At hospitals mainly photons (6-18 MV) and electrons (2-25 MeV) are used.
 - ❑ *Compared to clinical electron beams*: longer **penetration depth**; reduced **lateral scattering** (transversal widening \rightarrow sparing normal tissues).
 - ❑ *Compared to photons*: **scans** possible \rightarrow advantageous for image-guided energy- and intensity-modulated radiation therapy.
 - ❑ *Compared to protons*: greater **precision** of the beam, lower accelerator **cost**; less **radioprotection** issues.
 - ❑ *Biological advantages to be established !*

Conventional radiotherapy

❑ Conventional radiotherapy

- ❑ X-rays: 6 - 18 MV (tumors of all types)
- ❑ Electrons: 3 - 18 MeV (surface treatment)
- ❑ Machines: electron linear accelerators + multi-lame collimators (1-4 M€)
- ❑ Syst. quality control & imagers : advanced

- ❑ Dose rate: **30-70 mGy/s**
- ❑ Time fractionation: 2 Gy/session, 5 sessions/week, total dose: 40-70 Gy
- ❑ Field sizes: 4 cm² - 40 cm²
- ❑ Many items become « conventional »: experience 60 years in dosimetry, clinical effect of X-rays, dose control ...



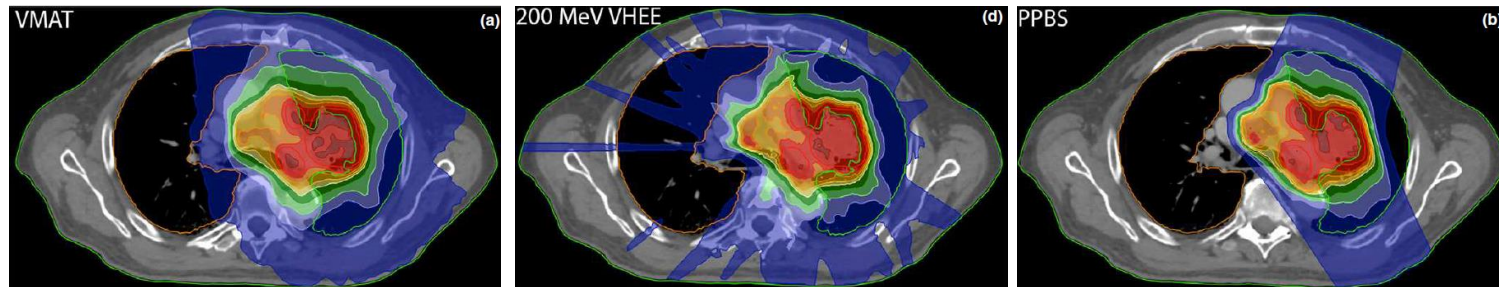
Conventional e- accelerator (X-rays 6-18 MV)

Radiobiology basics

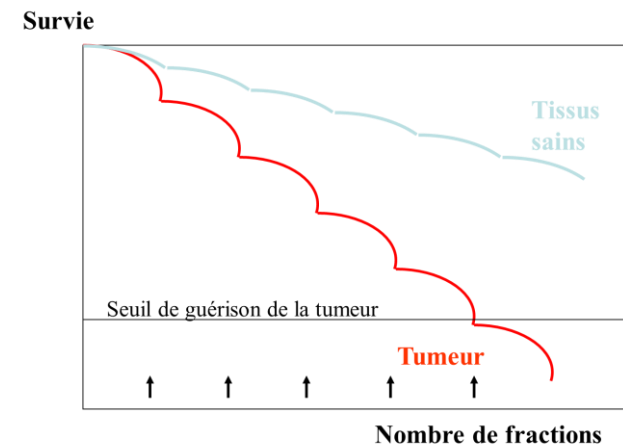
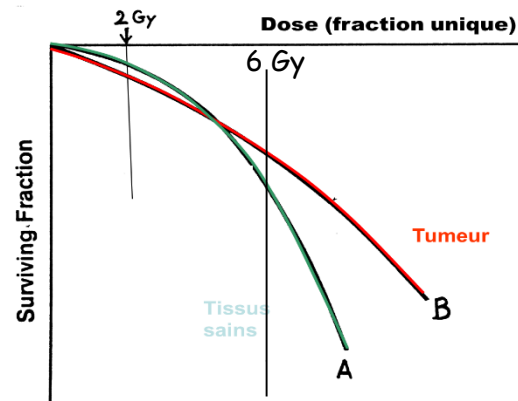
- Different effect for tumor and healthy tissues with:

Lung tumor : comparison X-ray, VHEE, & protons
Schuler, 2017 (Stanford)

- **Ballistic precision/ anatomic restrictions**



- Limits: precision of tumor limits, organ movements / repositioning errors, machine cost.
- **Dose deposit shape & time fractionation**
 - For the same total dose, biological efficiency differs according to dose/session, total number of sessions (fractionation) and treatment time (staggering)
 - Allows reparation of radiomolecular lesions and tissue repopulation
 - Allows tumor reoxygenation: reduces radioresistance of tumors

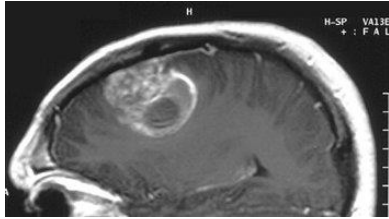


- **Pharmacomodulation:** combination of radiotherapy with chemotherapy, specifically acts on the cells of rapid proliferation (particularly tumors)

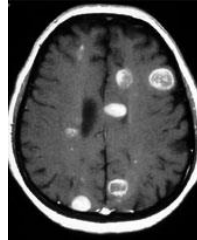
Radiotherapy, context

❑ Limits of conventional radiotherapy

Resistant, voluminous and diffuse cancers (glioblastomes)



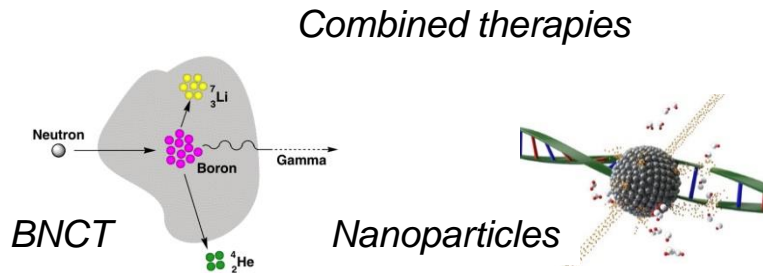
Non-localized tumors (multi-métastases)



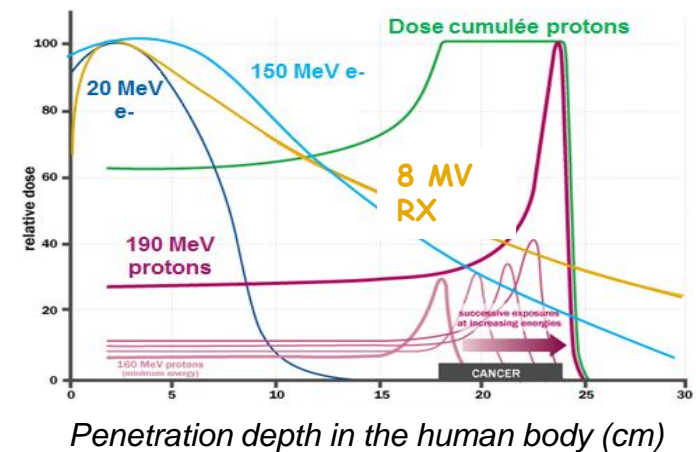
- ❑ Precision of tumor limits, organ movements, patient repositioning errors
- ❑ Toxicity to healthy tissues limits the dose

❑ How to improve the treatment?

- ❑ Induce more effective tumor irradiation → e.g. **hadrontherapy, combined therapy** with nano-particles/chemical agents

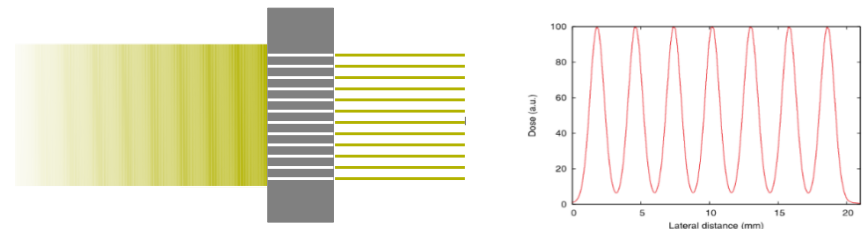


Different particles/energies



- ❑ Preserve healthy tissues via dose delivery mode: **microbeams & FLASH**

FLASH therapy, very high dose rate
> 40 Gy/s (conventional 0,03 Gy/s)



Spatial fractionation of the dose

- ❑ Impact of cost and congestion on the number of patients treated



*Hadrontherapy center in Heidelberg
(~Ten in the world, ~100 M€)*

VHEE ?
(~10 M€ ?)



*Standard medical accelerator
(~ 500 in France, ~1-4 M€)*



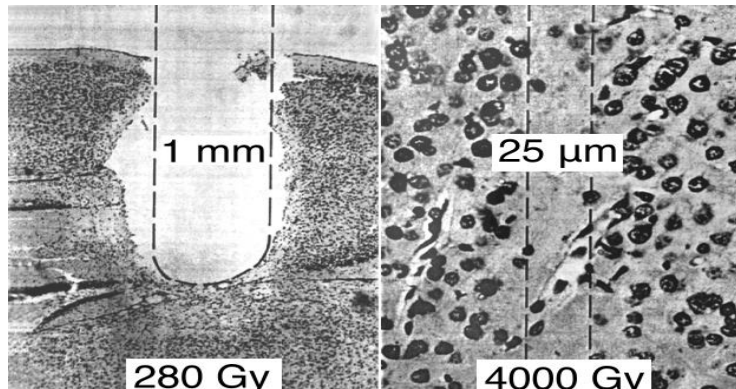
Challenge for quality control of the dose

- ❑ **VHEE beams: advantages vs protons**
 - ❑ Cost and beam handling, more compact accelerators
 - ❑ For our applications: very small beam sizes (<1mm)

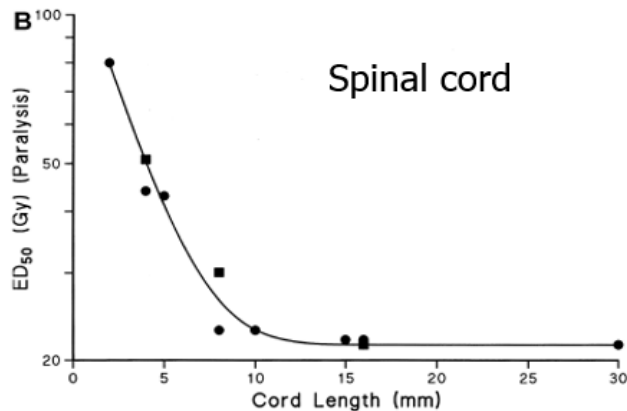
NARA (New Approaches in RAdiotherapy): Spatial fractionation of the dose

❑ Spatial fractionation of the dose and mini-beams

Very small field sizes ($< 1 \text{ mm}^2$)

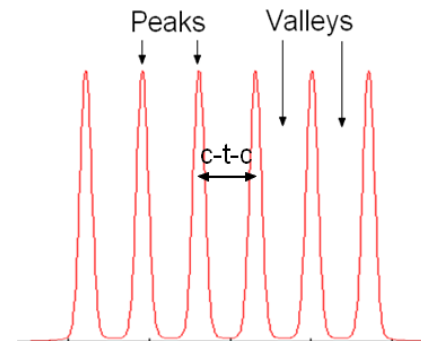
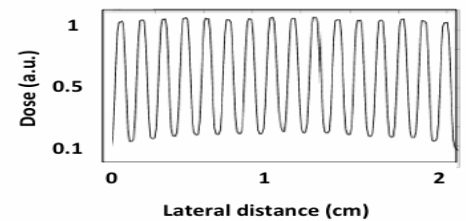
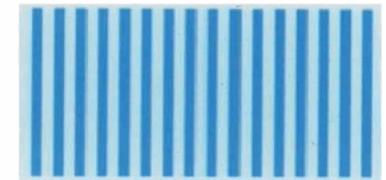
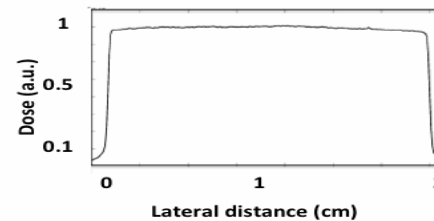
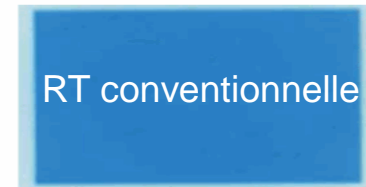


Zeman et al., Science (1959)



Hopewell et al.,
Radioth. Oncol.
(2000)

+ Spatial fractionation of the dose



$$PVDR = \frac{D_{\text{peak}}}{D_{\text{valley}}}$$

↗ PVDR = ↗
tolerance of
healthy tissue

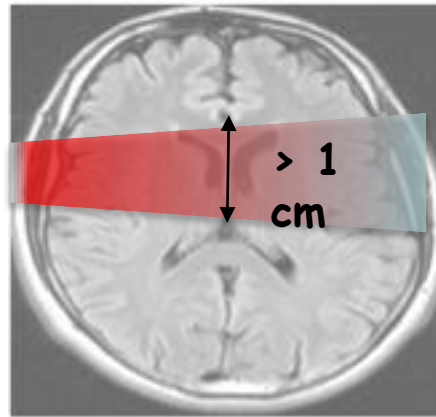
↘ D_{valley} to ensure
tissue integrity

Dose-volume effect: the smaller the field is, the higher dose tolerance of healthy tissues

NARA: Spatial fractionation of the dose

Standard radiotherapy

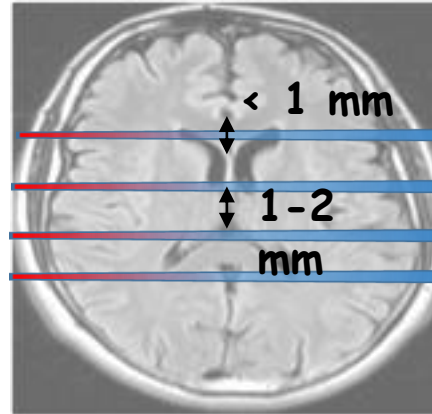
Large field sizes
($> 1 \text{ cm}^2$)
+
Homogeneous dose



Lethal dose $> 20 \text{ Gy}$

Fractionated radiotherapy: *x-rays mini-beams*

Small-size beams
spaced by the zones
of low dose
+
Heterogeneous dose



Biological mechanisms still
poorly known

❑ Remarkable increase in brain tolerance (100 Gy/session)

Prezado et al. 2015

❑ Possible dose increase \rightarrow better tumor control

❑ « Protective » effect of healthy tissues reproduced with **proton mini-beams** + tumor control increased with proton mini-beams compared to standard proton treatment

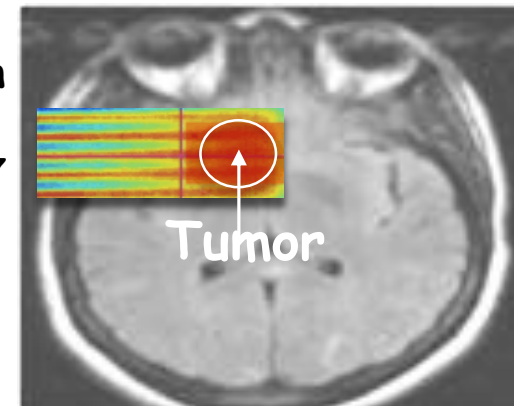
Prezado et al. 2017

Radiobiological effect of spatial fractionation :

❑ Cell repair and repopulation of zones « valley » \rightarrow zones « peak »

❑ Differential tissue effect between vascularization « immature » (tumor type, reparation --) and « mature » (healthy tissues)

Bouchet et al.



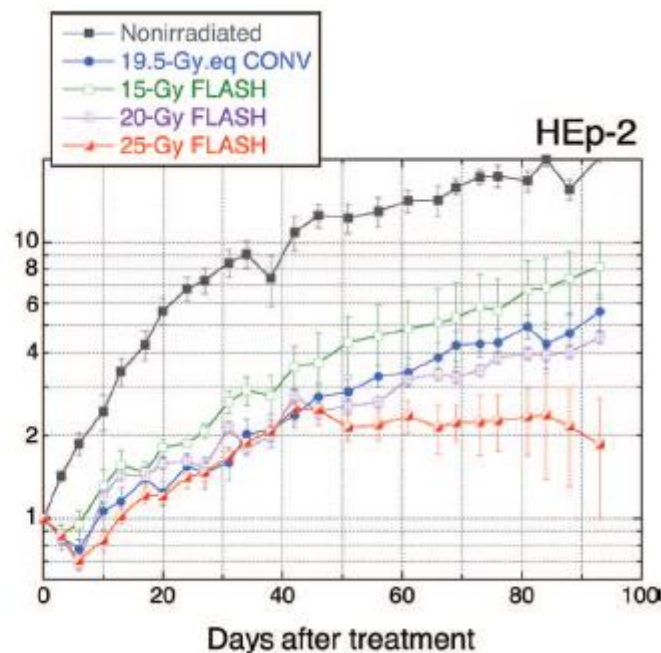
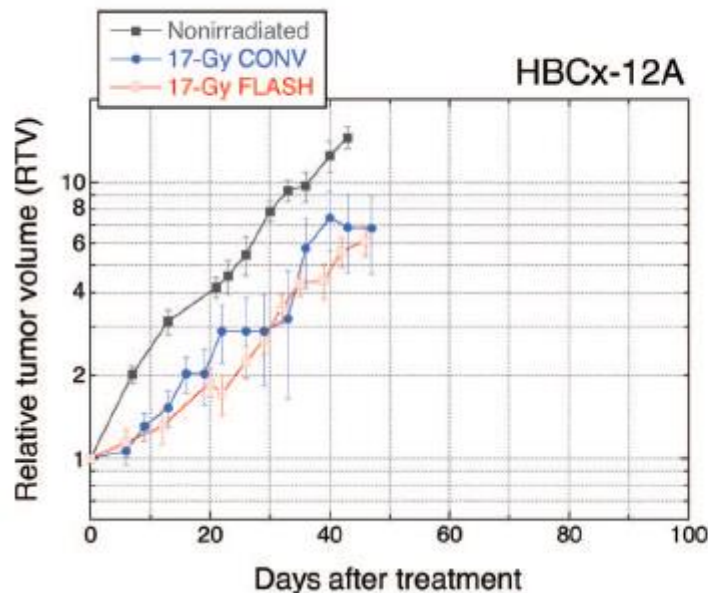
Ultrahigh dose-rate FLASH irradiation increases the differential response between normal and tumor tissue in mice

2014

Vincent Favaudon,^{1,2*} Laura Caplier,^{3†} Virginie Monceau,^{4,5‡} Frédéric Pouzoulet,^{1,2§}
 Mano Sayarath,^{1,2¶} Charles Fouillade,^{1,2} Marie-France Poupon,^{1,2||}
 Isabel Brito,^{6,7} Philippe Hupé,^{6,7,8,9} Jean Bourhis,^{4,5,10} Janet Hall,^{1,2}
 Jean-Jacques Fontaine,³ Marie-Catherine Vozenin^{4,5,10,11}

□ Appearance of Pulmonary Fibrosis on mice:

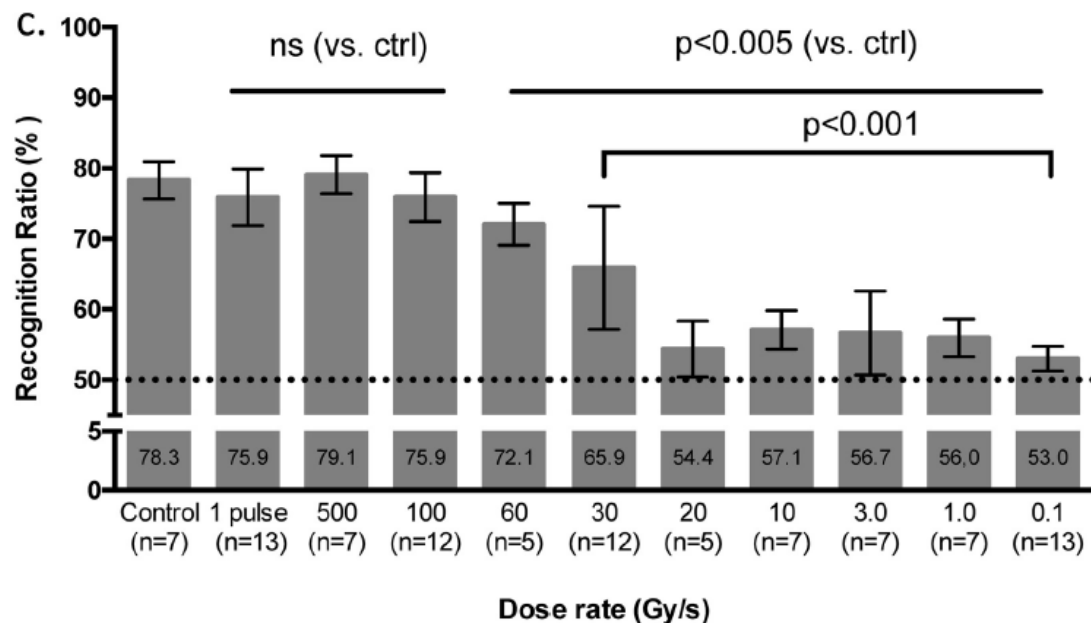
- Starting from 15 Gy in CONV mode (0.03 Gy/s).
- No fibrosis appearance in FLASH mode (40 Gy/s) up to 20 Gy + Protection of muscles and epithelial cells (skin, membranes...)
- Xenograft tumors on nude mice: **same tumor control** for CONV & FLASH
- → different effect tumor/healthy tissues !



2017

Irradiation in a flash: Unique sparing of memory in mice after whole brain irradiation with dose rates above 100 Gy/s

Pierre Montay-Gruel^{a,b,1}, Kristoffer Petersson^{c,1}, Maud Jaccard^c, Gaël Boivin^a, Jean-François Germond^c, Benoit Petit^a, Raphaël Doenlen^d, Vincent Favaudon^b, François Bochud^c, Claude Bailat^c, Jean Bourhis^{a,1}, Marie-Catherine Vozenin^{a,*,1}



Limit of a good effect at 100 Gy/s (or < 100 ms)

+ No effect if < 4 Gy unique dose

❑ Effect on the brain 50 Gy in FLASH mode equivalent to 10 Gy in CONV mode.

→ Biological effect ? Some oxygen process occurring very fast... (?)

PRAE: beam parameters and first simulation

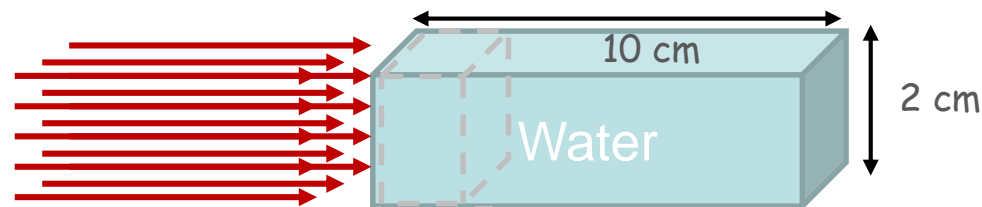
□ Beam at PRAE

- ✓ Small beam-size: $250 \mu\text{m} < \sigma < 2 \text{ mm}$
- ✓ Energies: 70 - 140 MeV
- ✓ Small divergence: 0.1 - 0.4 mrad
- ✓ Dose rate: $0.035 \text{ Gy/s} - 40 \text{ kGy/s}^*$

**depending on σ , Q*



□ First simulations to optimize the beam for VHEE:



(1)

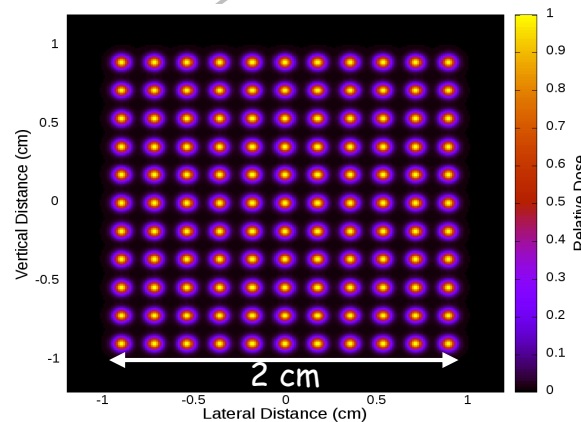
(2)

(2) $PVDR = 1$,
Favorable for tumor control

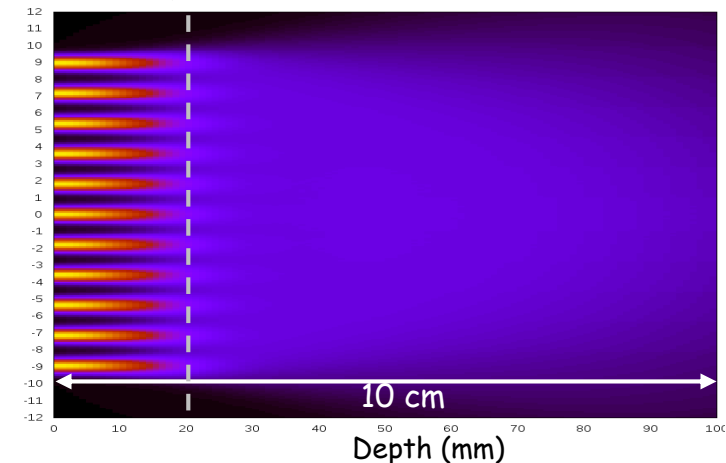
**Example: 70 MeV,
 $\sigma \sim 250 \mu\text{m}$**

**(1) $PVDR = 20$,
important spatial dose
fractionation**

$$PVDR = \frac{D_{\text{peak}}}{D_{\text{valley}}}$$



dose fractionation at the entrance



dose homogeneity with depth

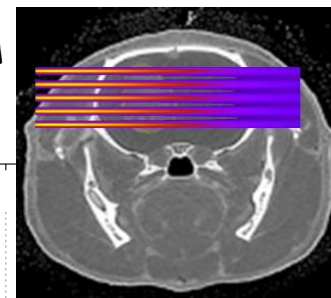
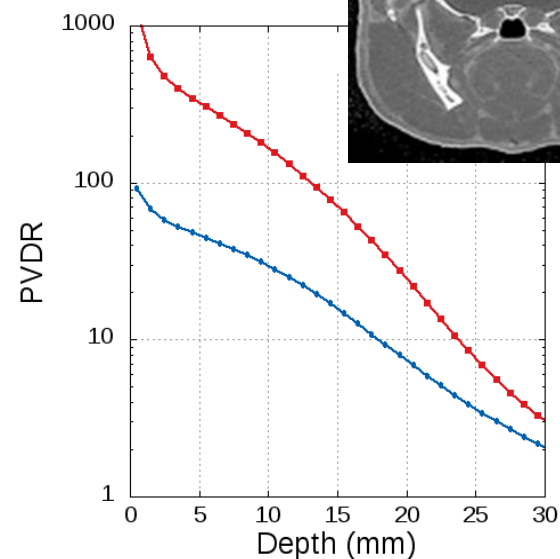
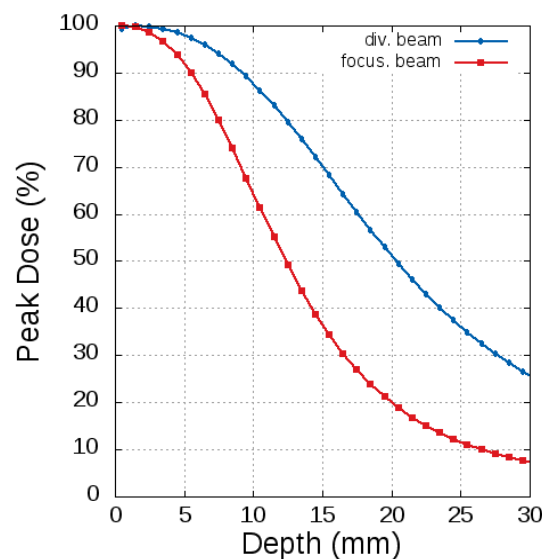
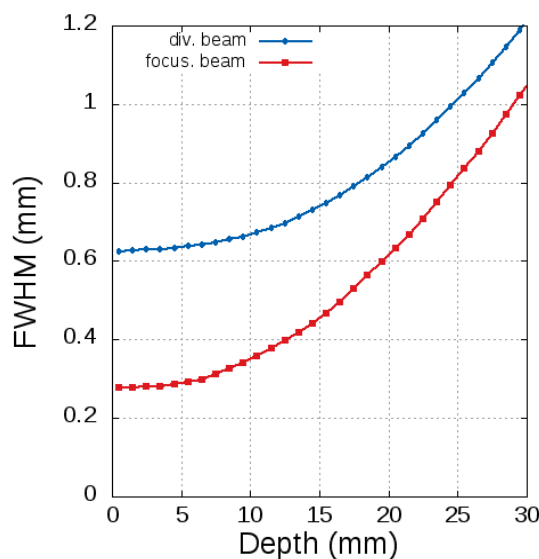
Optics optimization for PRAE

□ Beam size (FWHM) and dose rate at the phantom entrance (Gy/s , voxel $0.1 \times 0.1 \times 1 mm^3$):

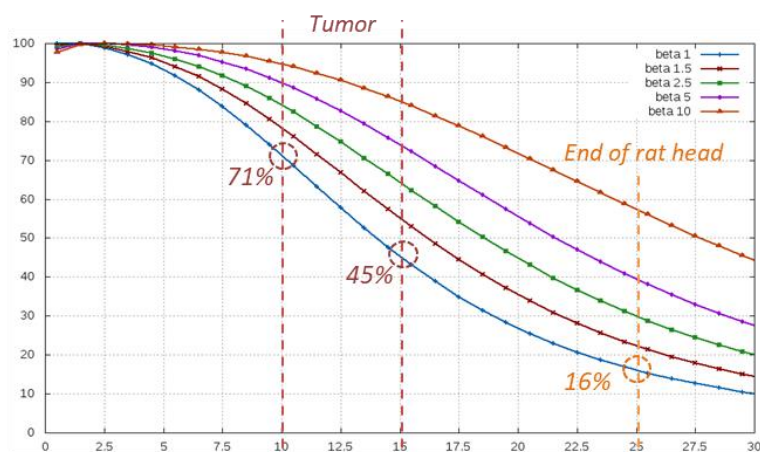
Energy	Beta/AG (cm)	FWHM	BWF	1 pC	2 nC
70 MeV	Beta1 – 10 cm	650 μm	1.15	18 Gy/s	36 kGy/s
	Beta 1 – 100 cm	11 mm	20	0.05 Gy/s	110 Gy/s
	Beta 120 – 100 cm	12 mm	2	0.037 Gy/s	70 Gy/s
140 MeV	Beta1 – 10 cm	600 μm	1.03	23 Gy/s	46 kGy/s
	Beta 1 – 100 cm	6 mm	9	0.25 Gy/s	500 Gy/s
	Beta 120 – 100 cm	6.1 mm	1.06	0.2 Gy/s	400 Gy/s

*Conventional = 0.033 Gy/s

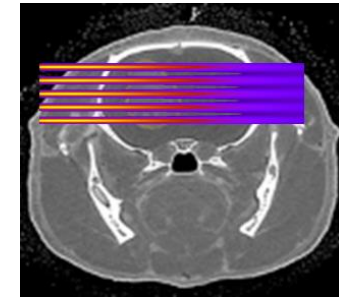
□ PRAE settings: beam pipe window - 10 cm of air - 3 cm depth in phantom



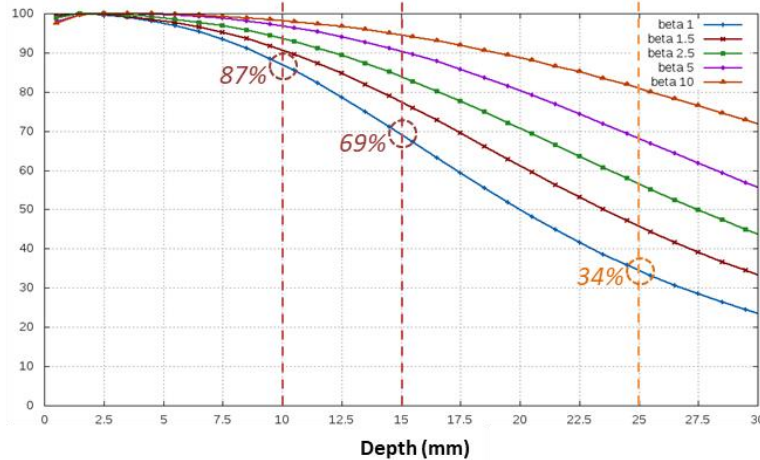
Percentage depth dose (peak)



70 MeV



Percentage depth dose (peak)



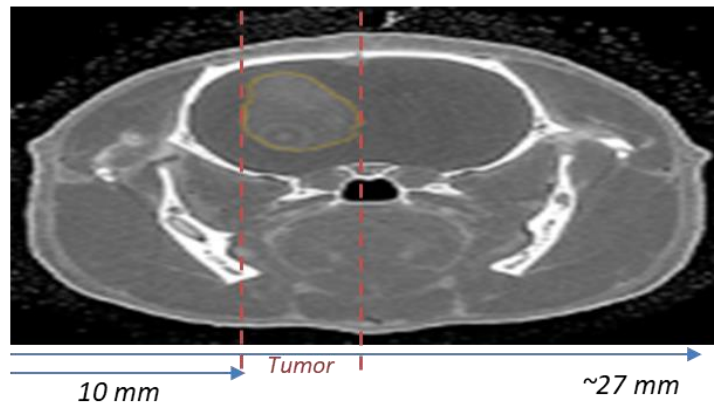
140 MeV

With 140 MeV, σ 250 μm (SFR):

- submillimetric over all depth
- dose sufficiently large to control a tumor

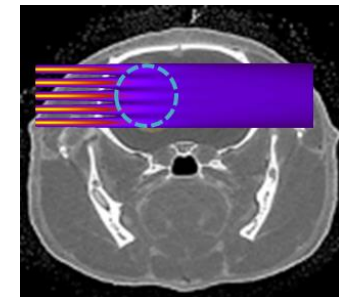
With 70 MeV, σ 350 μm (partial SFR)

- submillimetric < 10 mm
- dose homogeneous in tumor

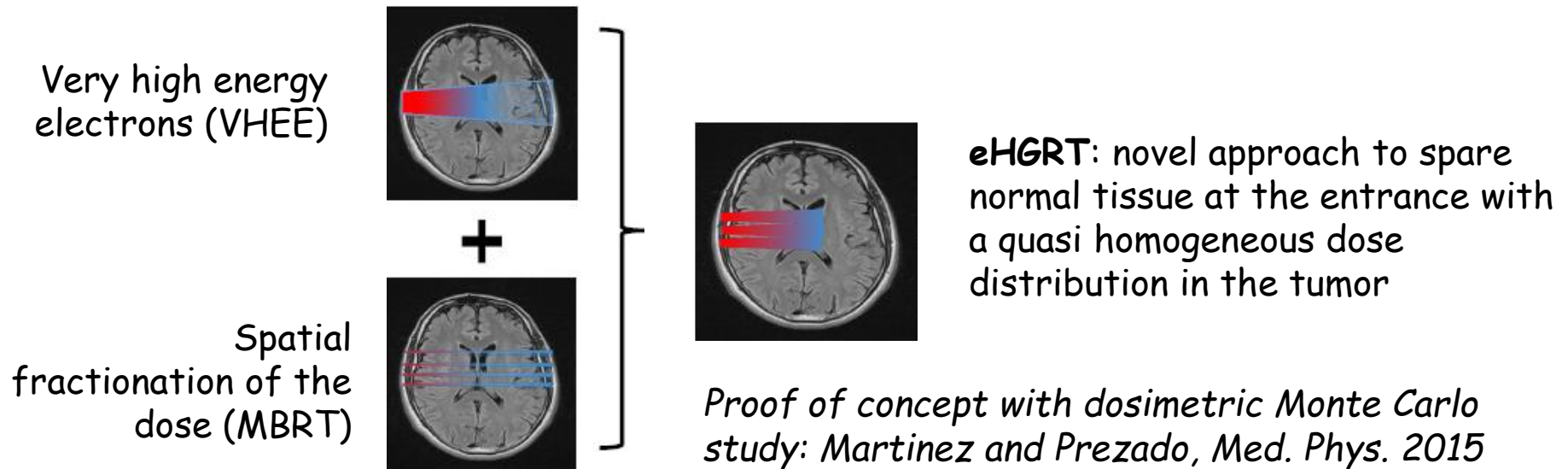


Example of rat head
with a brain tumor

Typical depth of
interest



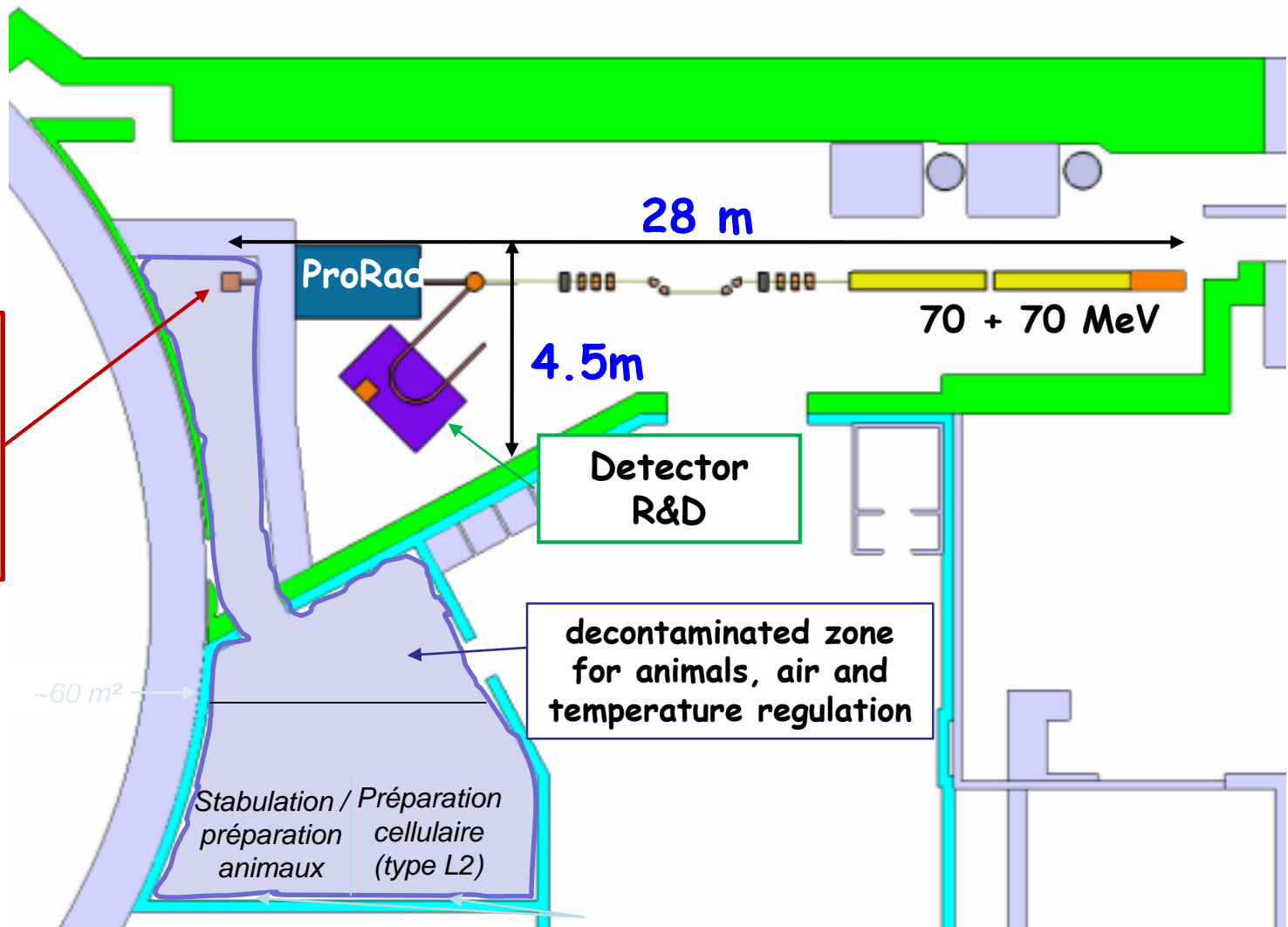
☐ High Energy Electron Grid Therapy (eHGRT):



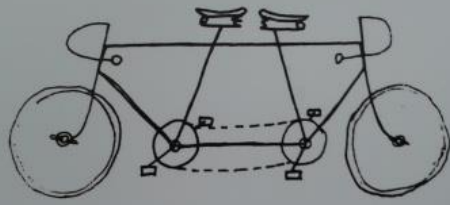
☐ To be studied on the PRAE radiobiology line:

- ☐ *Experimental dosimetry for very small field sizes:* with radiochromic films and microdiamond detector
- ☐ *Monte Carlo dose calculation:* beam characteristics for eHGRT, validation of experimental dosimetry, dose calculation for radiobiology studies
- ☐ *Radiobiology studies on cells and small animals:* confirmation of the hypothesis of high normal tissue resistance
- ☐ Relative Biological Efficiency (RBE) of VHEE with respect to photons
- ☐ « FLASH » effect
- ☐ Online imaging/control

Experimental area



*Preparation hall for biological experiments
(animal room by Curie Institute)*



Bruno Touschek

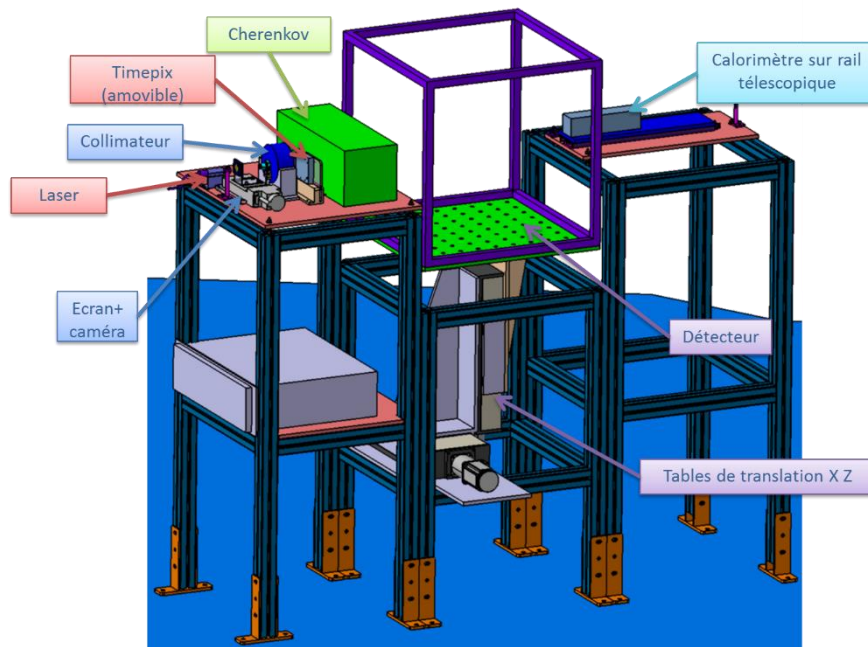
Instrumentation R&D

- ❑ *Principle goal is to construct versatile tool for detector R&D and tests:
deliver calibrated beam with adjusted and known kinematics and number
of electrons per sample*

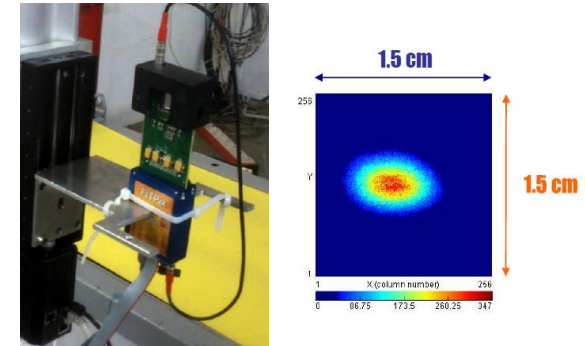
- ❑ **Fully-equipped versatile tool for precision instrumentation R&D based on high-performance electron beam**
- ❑ **Excellent technical performance**
 - ❑ **Timing** reference, < 10 ps bunch length
 - ❑ **Charge accuracy**, $\text{RMS} < 2 \times 10^{-3}$
 - ❑ Low straggling (energy $\gg 1$ MeV)
- ❑ **High-performance, remotely controlled tools**
 - ❑ **Beam position, profile and monitoring**
 - ❑ 60 digitization channels for users on NARVAL-based **data acquisition**
 - ❑ Motorized **moving table for scans**, accuracy $< 500 \mu\text{m}$
- ❑ No need to place the detectors in vacuum

Measure the time, charge and imaging performance of particle detectors
→ Calibration for charge, trigger, tracking detectors

Instrumentation R&D at PRAE

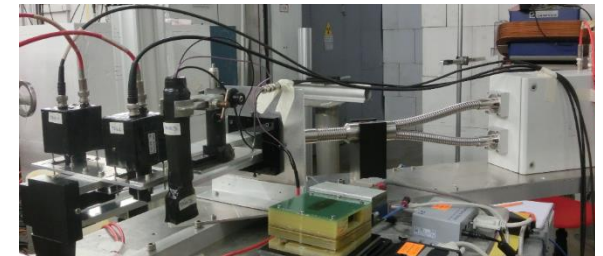


Timepix detector for precision spot measurement



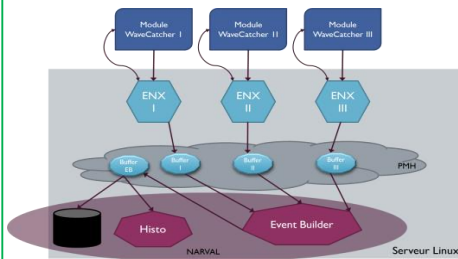
Cherenkov quartz counter for intensity monitoring

2 channel Cherenkov counters (LAL) tested at BTF (Frascati); installed in the SPS (CERN) beam pipe



DAQ + slow control

- ❑ 60 user digitization signals (WaveCatcher)
- ❑ DCOD = NARVAL + ENX



Participation of
Centre de Sciences
Nucléaires et
de Sciences de la Matière

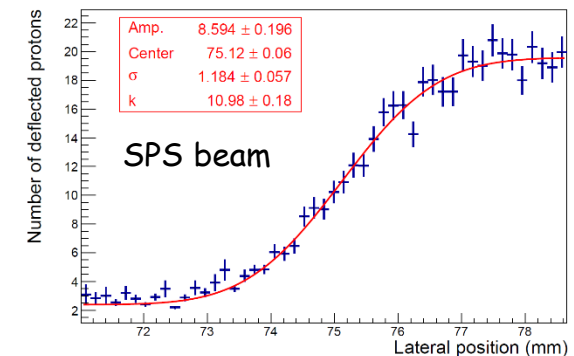


Calorimeter for energy monitoring

BGO scintillator crystals
in compact matrix geometry

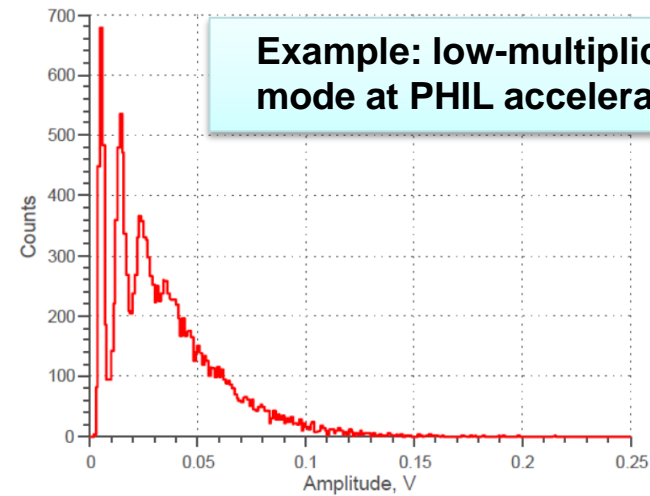
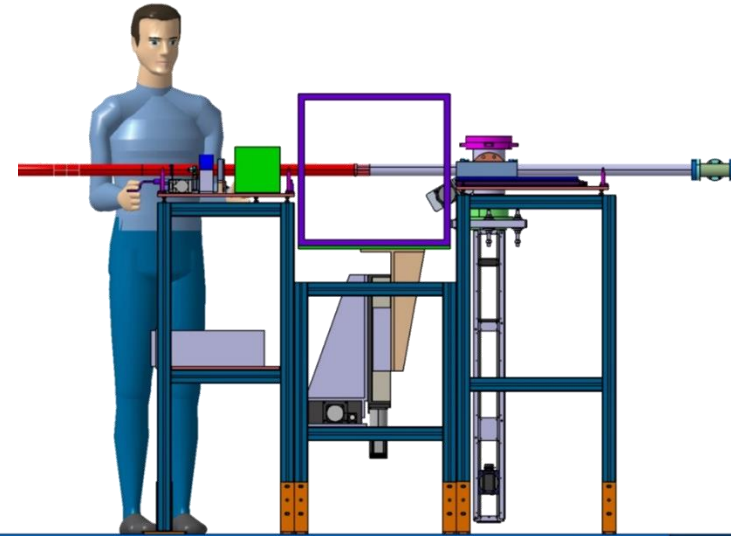
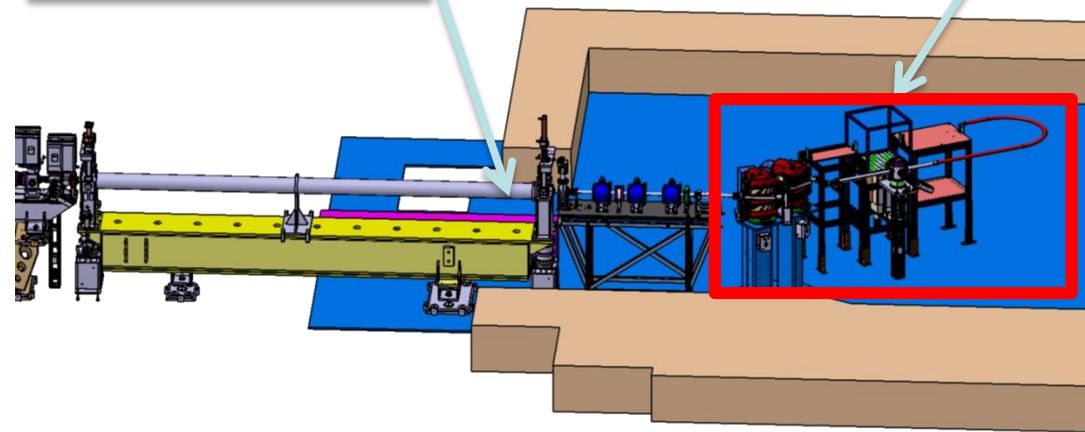


Example of a calorimeter realized at IPN



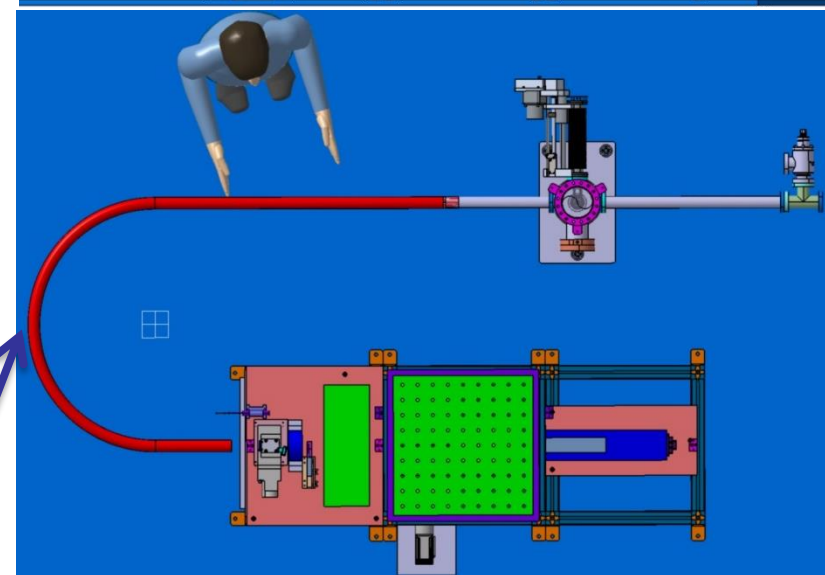
Ligne accélératrice

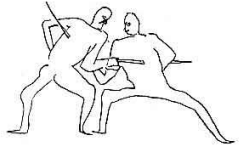
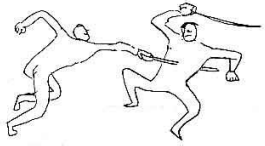
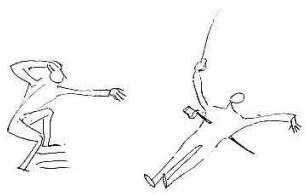
Plateforme



Example: low-multiplicity mode at PHIL accelerator

SPECTROMETER



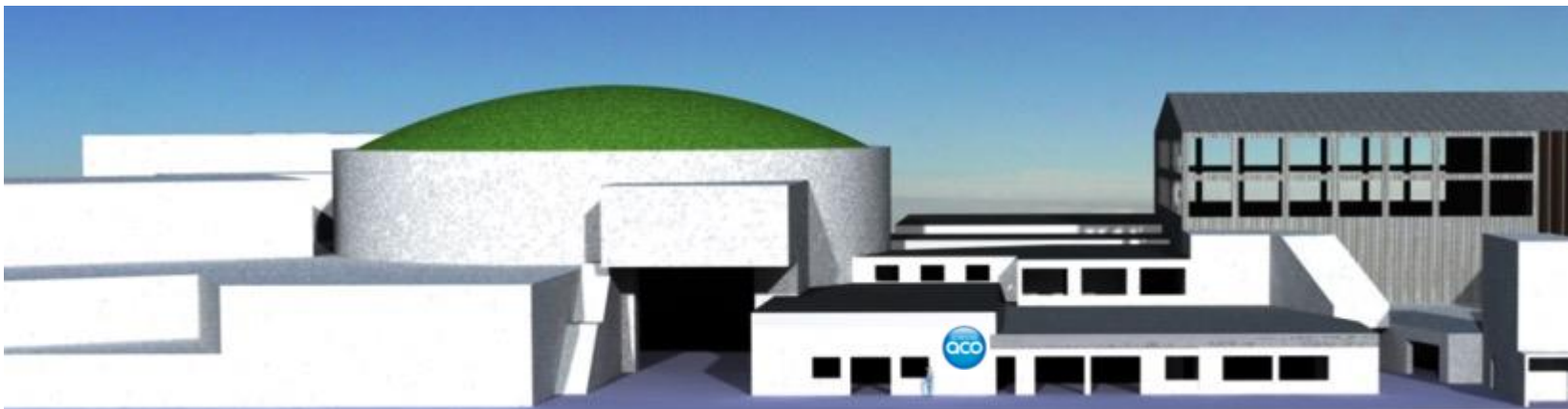
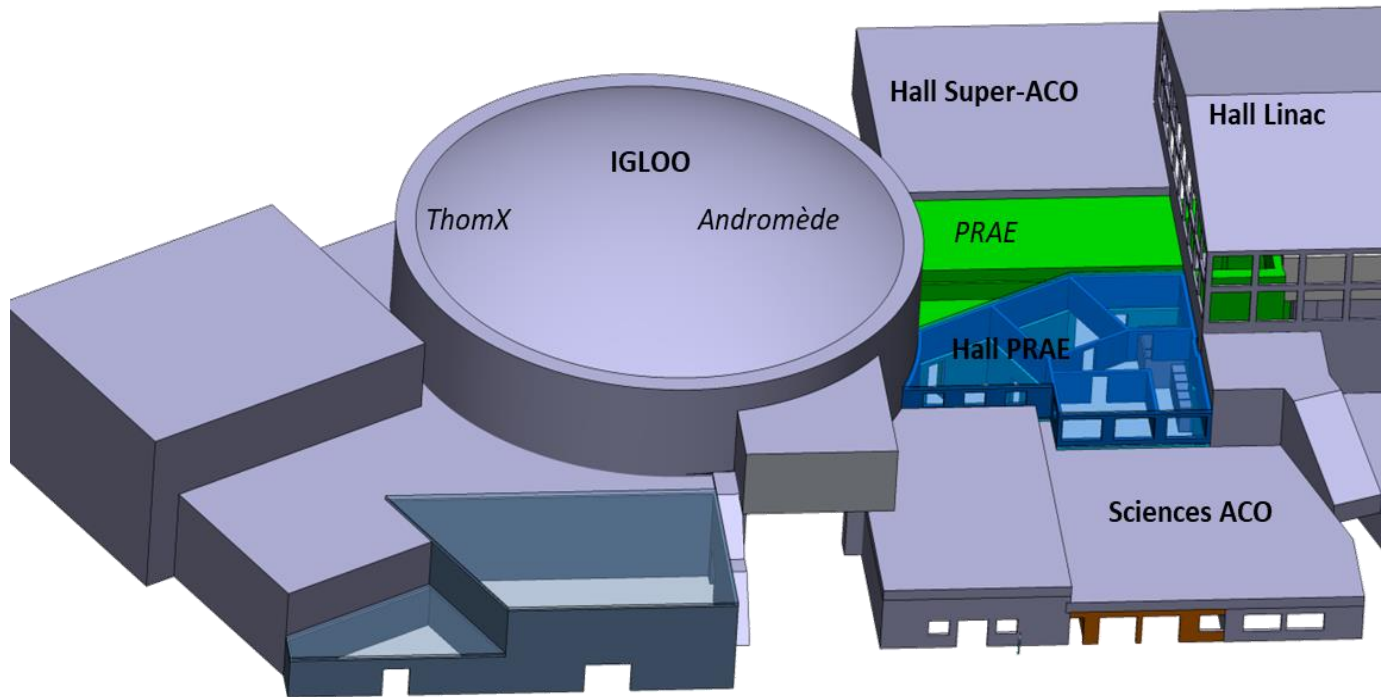


Bruno Touschek

PRAE site

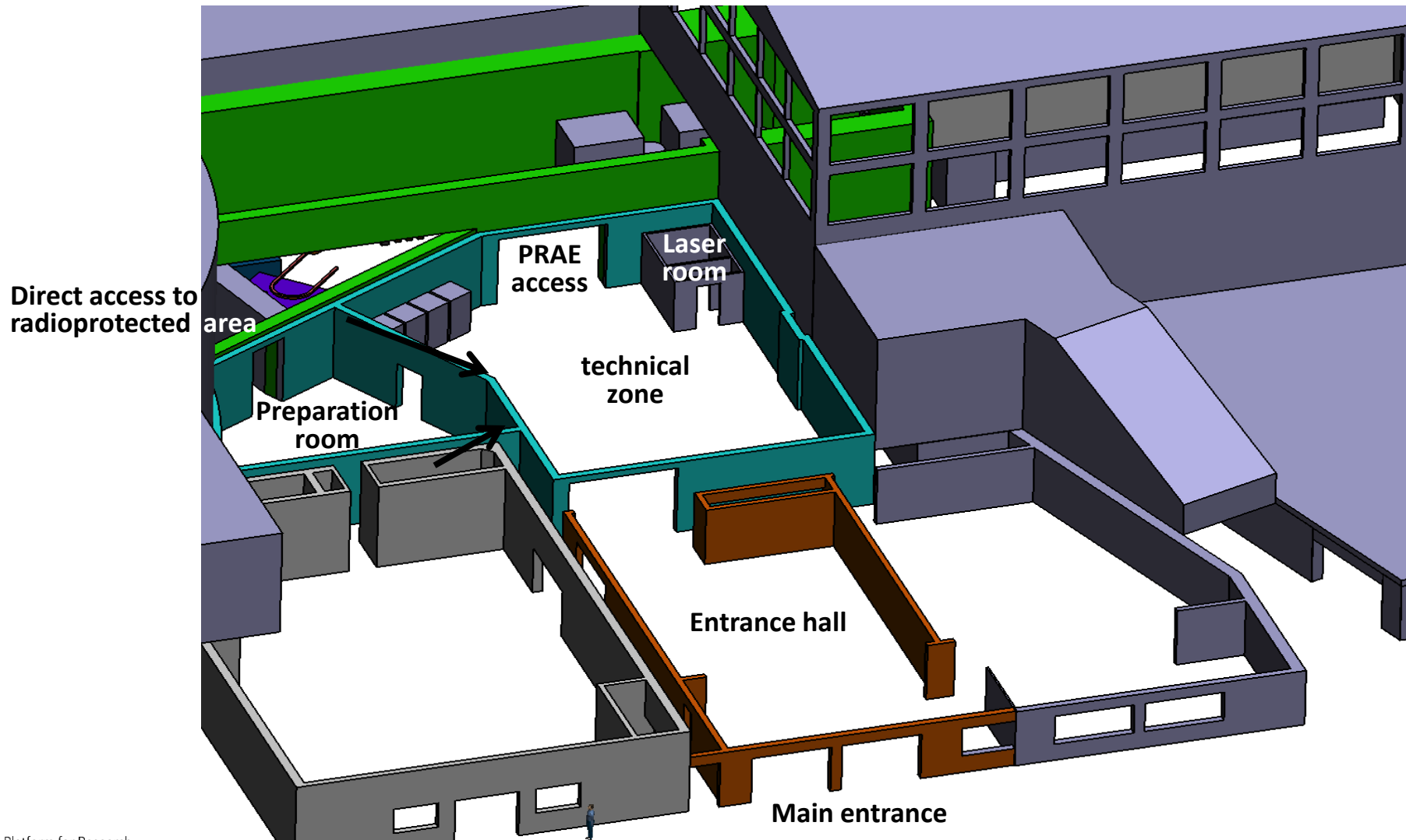
Future PRAE site: IGLEX complex

- ❑ PRAE experimental hall - existing structure, locked and radio-protected site



Ground floor of new building

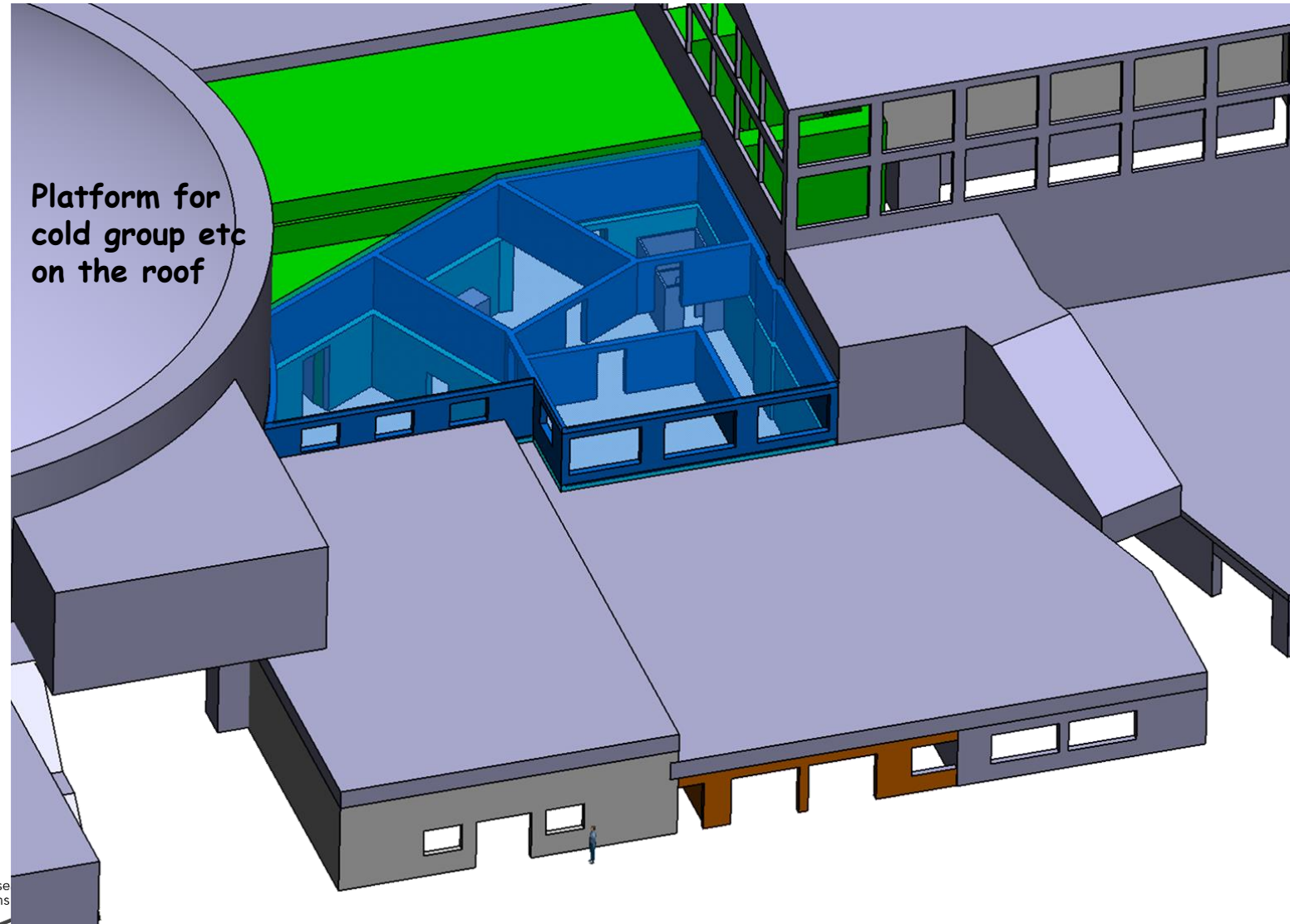
Ground surface : 290 m²



PRAE site layout

1st floor of new building

- ☐ Control and acquisition room
- ☐ Additional equipment



Summary

- ❑ PRAE is a new project for science, R&D and applications based on **complementary expertise of major Orsay laboratories.**
- ❑ Construction of the multi-disciplinary PRAE site - Subatomic physics, Radiobiology, Instrumentation R&D and Accelerator - is centered around the **new high-performance electron accelerator.**
- ❑ We expect a start of the main PRAE program in 2020-2021.
- ❑ The PRAE collaboration is open to new groups:
YOU ARE WELCOME TO JOIN !



Bruno Touschek

Backup

European facilities, table

(this worksheet is now protected, please contact Enk Adli if you have modifications/corrections.)	EUROPE (only primary beams)									
Name	CALIFES	CLARA	FlashForward	Sinbad	PITZ	SPARC_LAB	Max IV injector	PRAE	RADEF (clinac)	FLUTE
Country	Switzerland	UK	Germany	Germany	Germany	Italy	Sweden	France	Finland	Germany
Laboratory	CERN	Daresbury	DESY, Hamburg	DESY, Hamburg	DESY, Zeuthen	INFN, Frascati	Max IV	Orsay, France	Jyväskylä	KIT
Type of facility	TBD	Test facility for UKFEL R&D	DESY tests of PWFA	Adv. accel. research	Photo-inj test facility	Adv. accel. research	Part of Max IV. Ideas (but no funding) to create a 3 GeV ebeam test facility	Multi-disiplinary	Medical linac (?)	THz tests
Online when?	Online	Jan 2017 (50 MeV)	mid-2017	2018 ?	Online	Online	Linac under final commissioning. Parameters as expected when fully commissioned.	2020 ?	online	online (?)
Energy	130-200 MeV (60 with upgrade)	50 MeV (Jan 2017) 250 MeV (Sept 2019)	1.25 GeV	100 MeV	25 MeV	150 MeV	3 GeV	65 MeV	<= 20 MeV	41 MeV
Energy spread	< 1 MeV FWHM (< 0.2 % rms)	25 to 100 keV rms	0.10%	< 0.3% (low charge, peak)	<0.5%	0,1%	<0.05% + chirp	0.2 % rms		
RF Frequency	3 GHz	3 GHz		3 GHz	1.3 GHz	2.856 GHz	3 GHz	3 GHz		
Rep. rate	1 or 5 Hz (25 Hz with upgrade)	100Hz at 250MeV, 400Hz at 100MeV	10 Hz	10 - 50 Hz	10 Hz	10 Hz	10 (100) Hz	50 Hz		10
Time structure	1.5 GHz, or single bunch	single bunch	single or double bunch	single bunch	up to 600 bunches at 1 MHz rep rate	single bunch or up to 4 bunches at 1 THz rep rate		single bunch		single bunch (?)
Bunch length	4 ps FWHM (~ 500 um rms)	35 fs to 1.9ps FWHM	10-500fs	sub-fs - 2 fs (low charge)	Flat top, 2ps rise/fall time; 22ps FWHM	30 fs - 5 ps	10-500 fs	10 ps		1 - 300 fs
Charge per bunch	10 pC to 0.5 nC (for < 30 bunches)	25 to 250pC	250 pC	0.5 pC - 20 pC for fs bunch 1 nC possible	20 pC to 4 nC	0.1-0.8 nC	20-200 pC	sub pC - 2 nC		1 - 3000 pC
Trans. emittance Normalized	3 um for 0.05 nC bunches, 20 um for 0.4 nC	0.5 to 1.0um	2 um	< 0.5 um	0.6 um for 1 nC	1 um	< 1um	3 - 10 um		

❑ « Biological » dose vs. « physics » dose

❑ Molecular scale:

- ❑ LET: ionisation density
- ❑ Reparation mechanisms ...

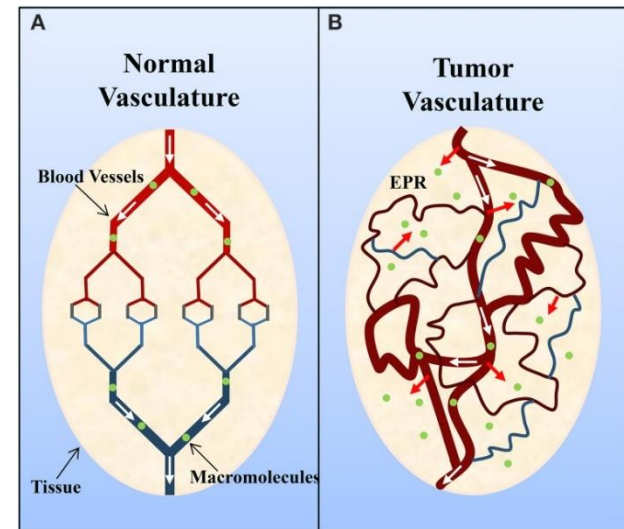
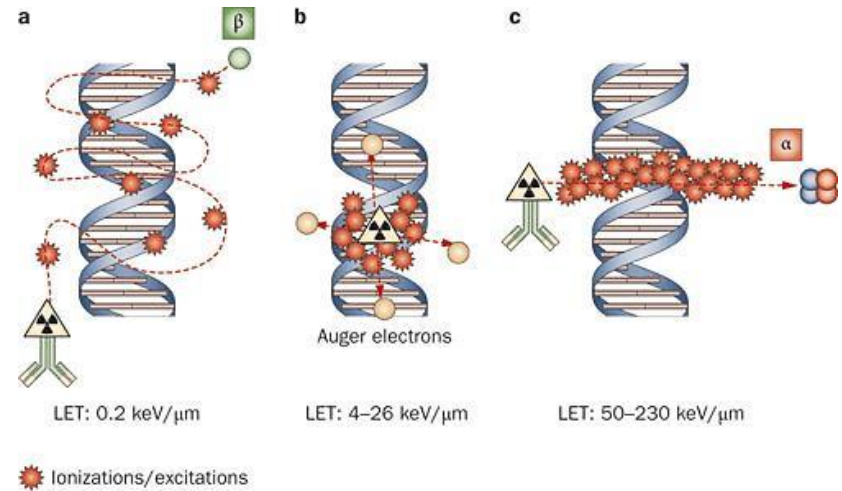
❑ Cellular / tissue scale

- ❑ Cellular regulation
- ❑ Vascularisation...

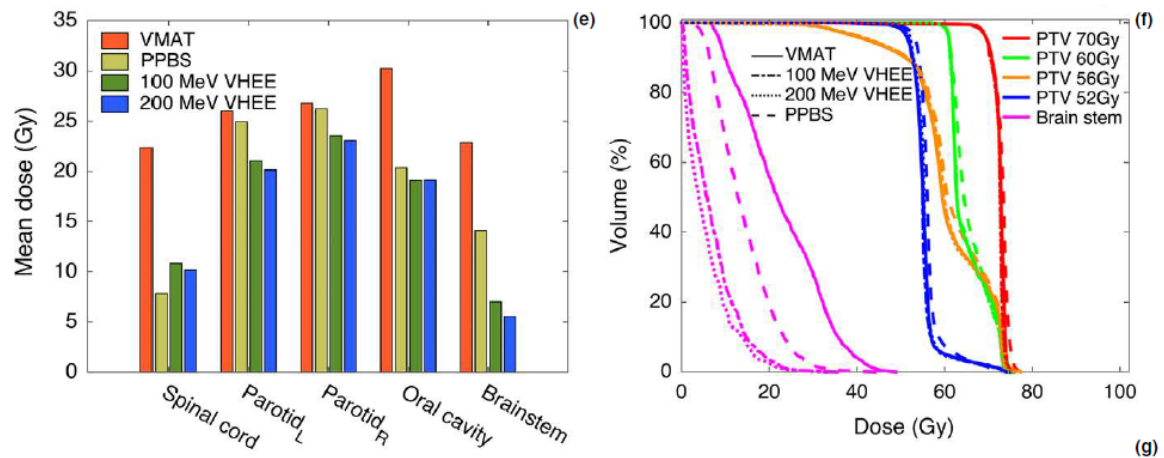
❑ Optimize physics parameters to induce different biological response

- ❑ Particles
- ❑ Dose delivery mode: temporal, spatial

❑ Objective: favorable difference between healthy tissue and tumor



Avantages VHEE, hétérogénéités, cas cliniques



Schuller 2017:
comparaison VHEE vs
protons et photons,
H&N cancer

FIG. 6. Treatment plan comparison, HNC. Treatment planning comparison between VMAT, PPBS, 100 MeV VHEE, and 200 MeV VHEE plans. (a-d) Coronal images through PTV for the different modalities, (e) mean doses to the spinal cord, parotid glands, oral cavity, and brain stem, (f) dose volume histogram for the PTVs and brain stem, and (g) mean integral body dose, conformity index, and homogeneity for the different modalities. [Color figure can be viewed at wileyonli-

Agnese Lagzda : avantage hétérogénéités

DesRosiers et al. 2008 : hétérogénéité

200 MeV VHEE

150 MeV protons

6 MeV photons

